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Berme et al.

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(54) **MOVEMENT ASSESSMENT APPARATUS AND
A METHOD FOR PROVIDING
BIOFEEDBACK USING THE SAME**

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(*) Notice: Subject to any disclaimer, the term of this
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U.S.C. 154(b) by 0 days.

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A61B 5/00 (2006.01)
G06F 19/00 (2011.01)
A61B 5/11 (2006.01)

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A61B 5/742 (2013.01); **A61B 5/7405**
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See application file for complete search history.

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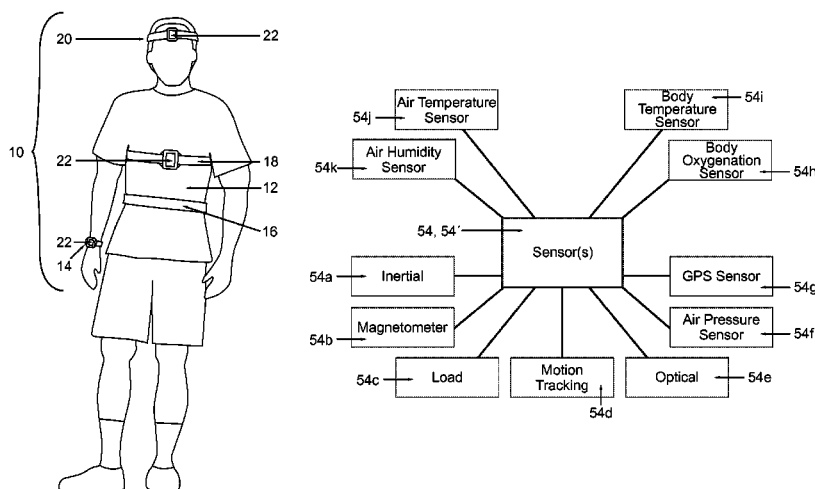
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(57) **ABSTRACT**

A movement assessment apparatus configured to provide bio-feedback to a user regarding one or more bodily movements executed by the user is disclosed herein. The movement assessment apparatus generally includes a sensing device comprising one or more sensors, a data processing device operatively coupled to the sensing device, and a sensory output device operatively coupled to the data processing device. The data processing device is configured to determine a movement path and/or velocity profile of the body portion of the user using one or more signals from the one or more sensors, to compare the movement path and/or the velocity profile determined for the body portion of the user to a respective baseline movement path and/or velocity profile, and to determine how closely the movement path and/or the velocity profile determined for the body portion of the user conforms to the respective baseline movement path and/or baseline velocity profile.

27 Claims, 22 Drawing Sheets



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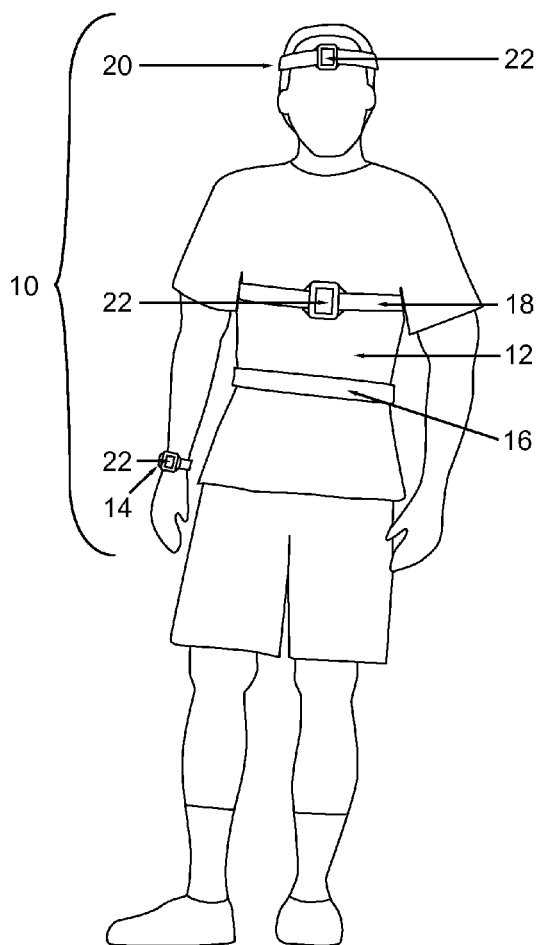


FIG. 1

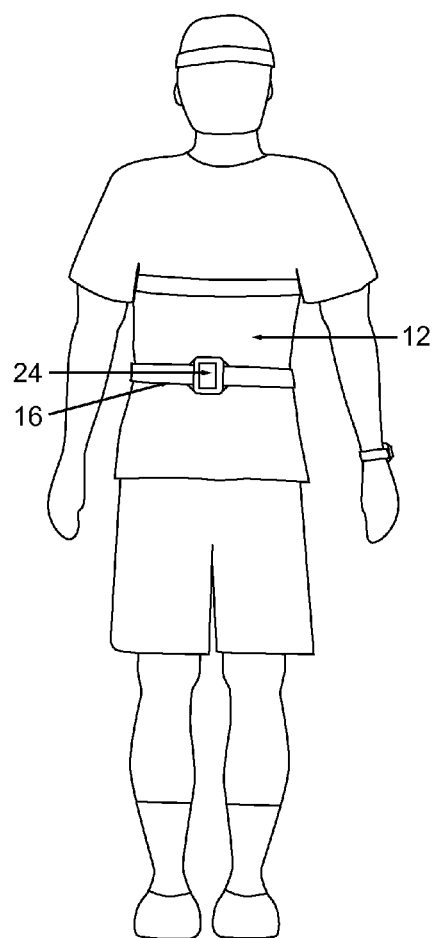


FIG. 2

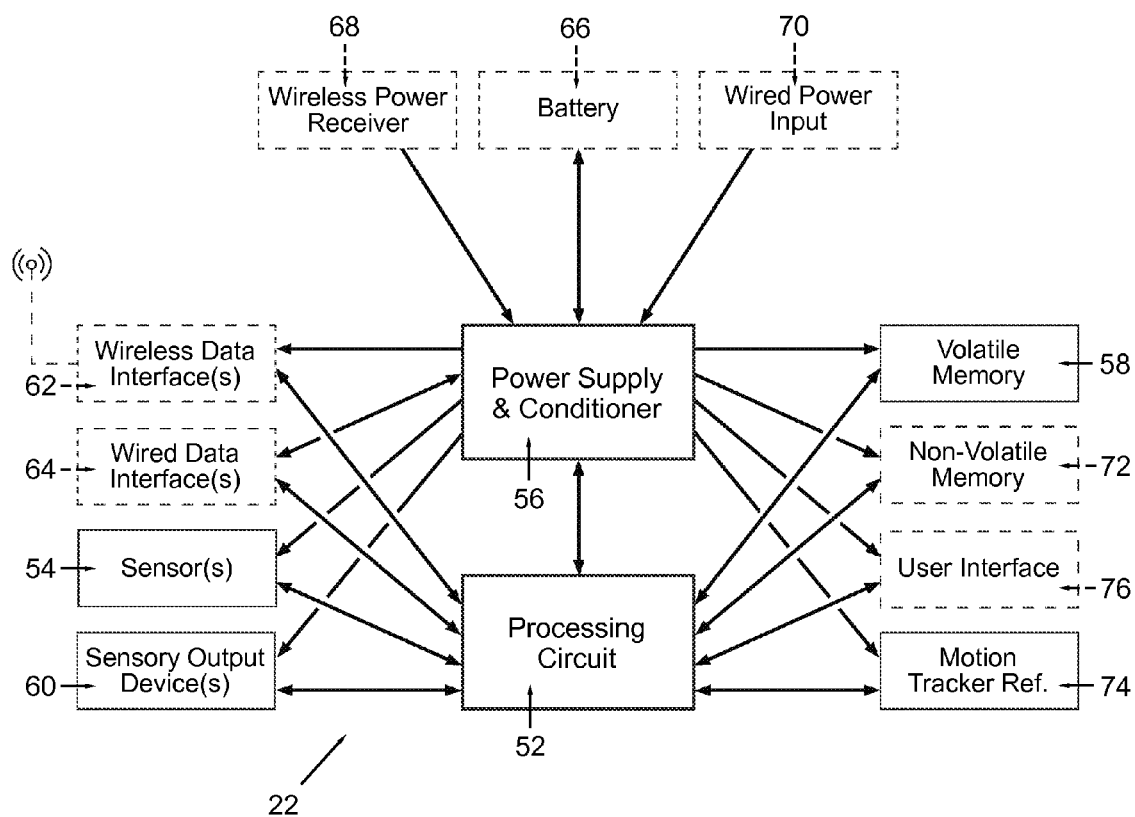
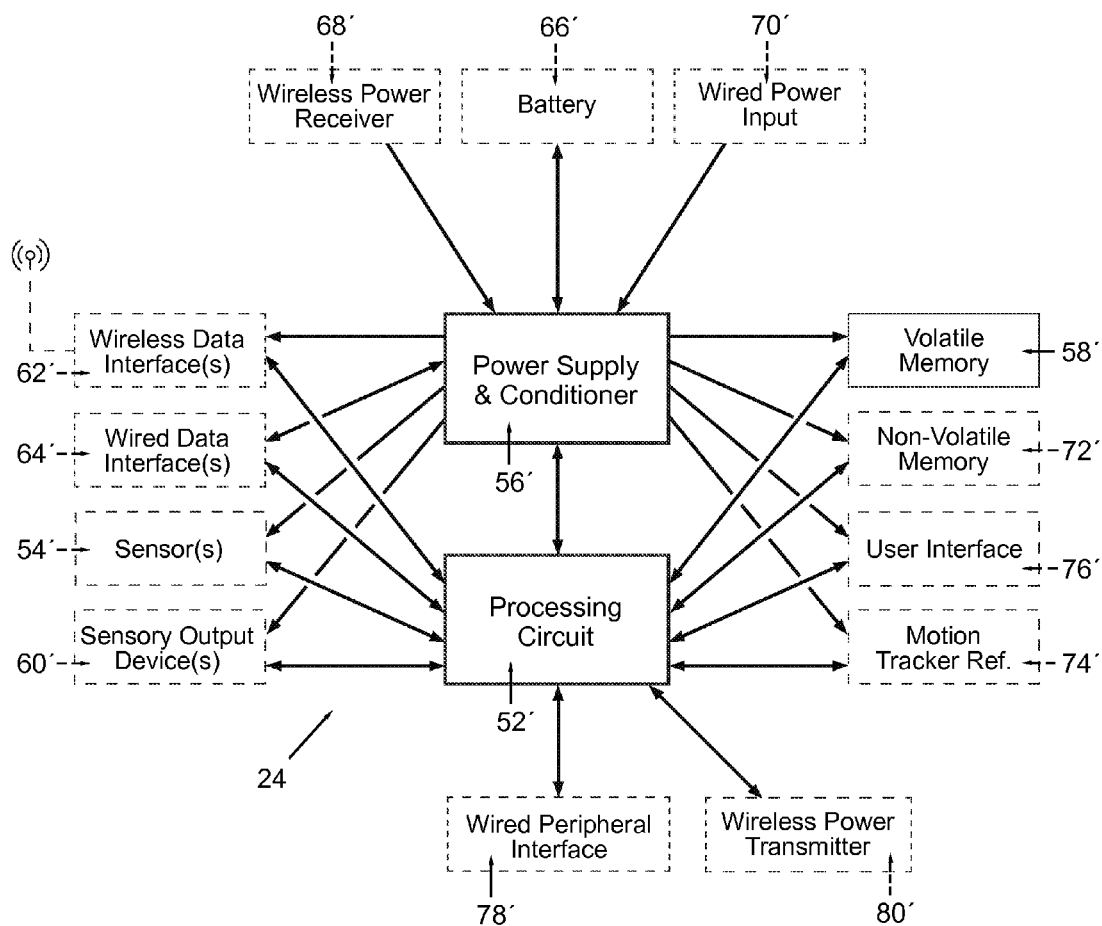
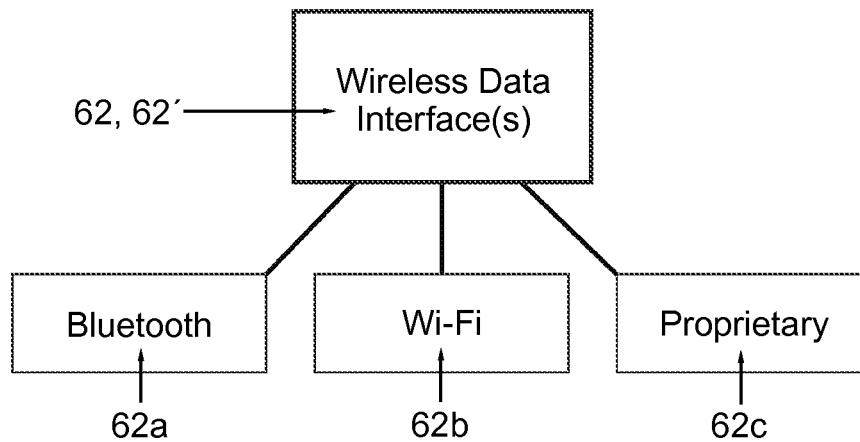
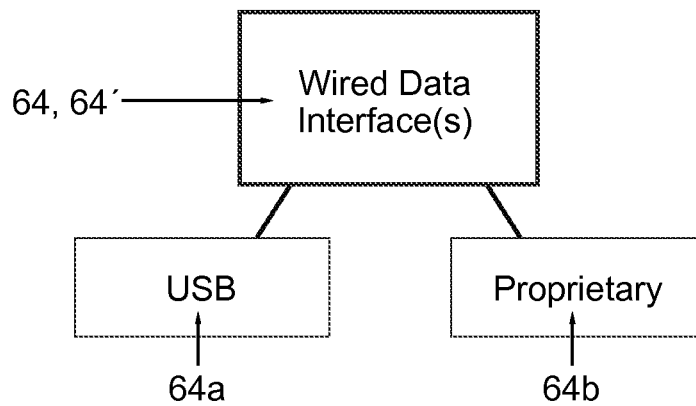
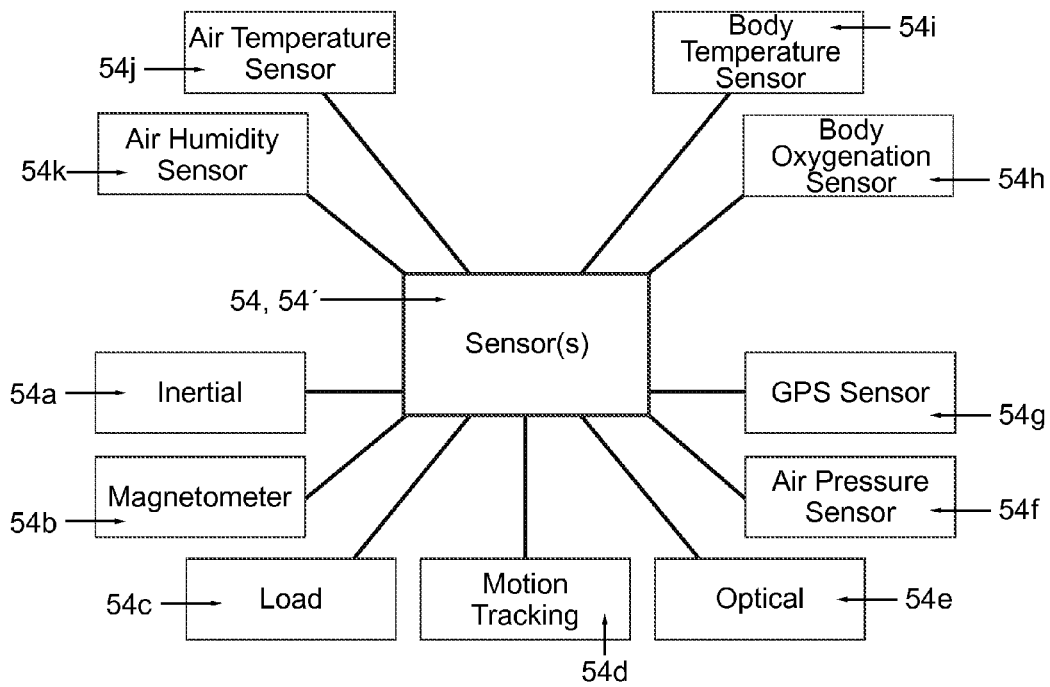
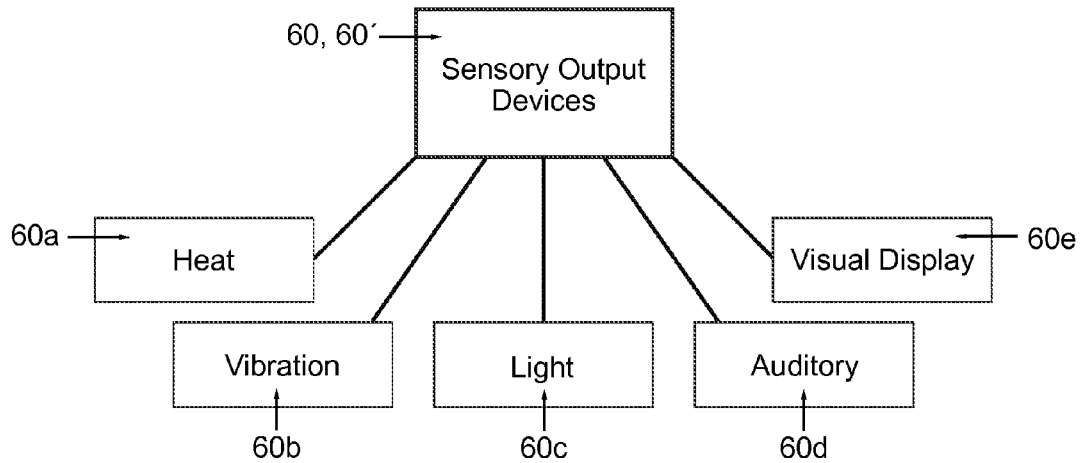
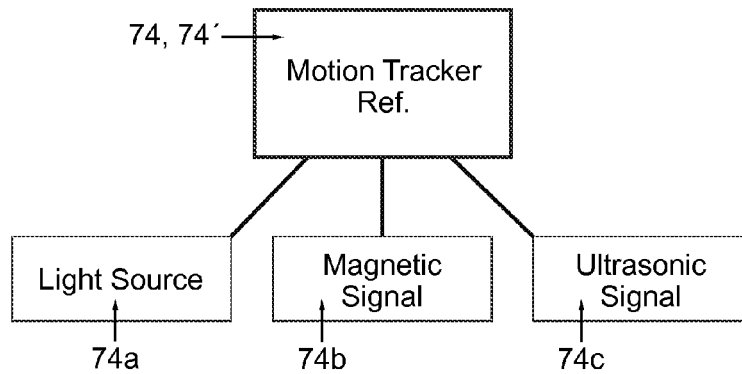
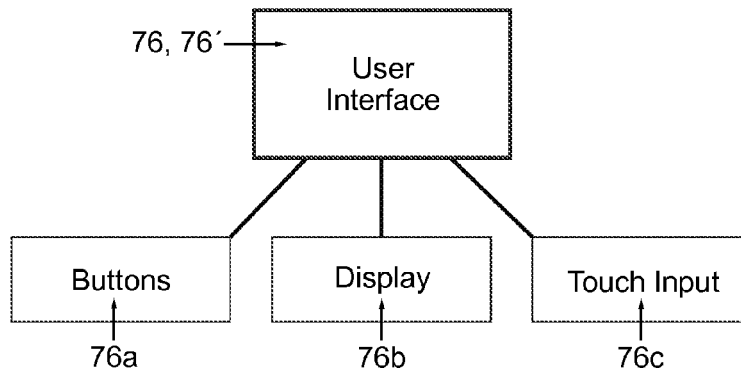


FIG. 3

**FIG. 4**

**FIG. 5****FIG. 6**

**FIG. 7**

**FIG. 8****FIG. 9****FIG. 10**

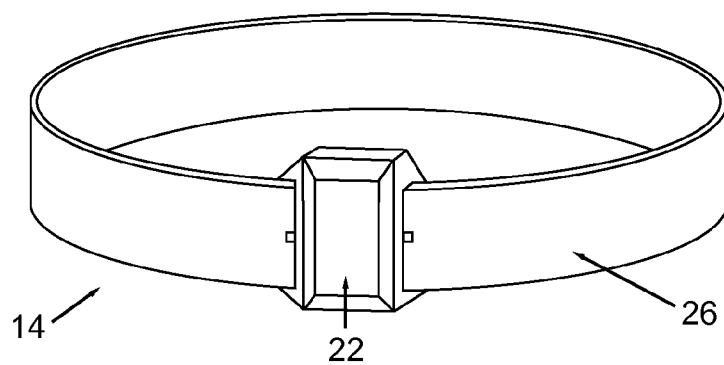


FIG. 11

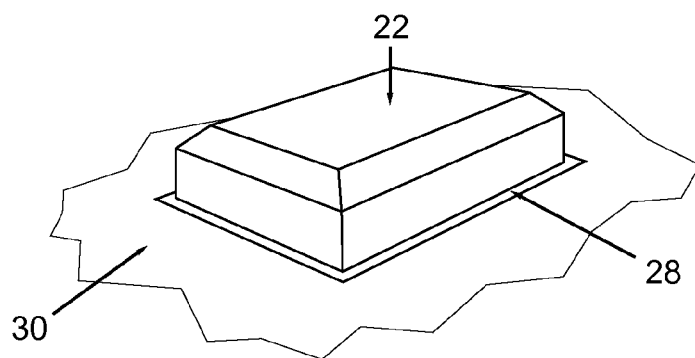


FIG. 12

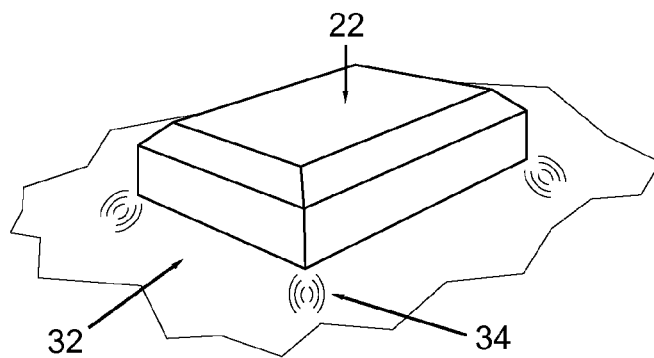


FIG. 13

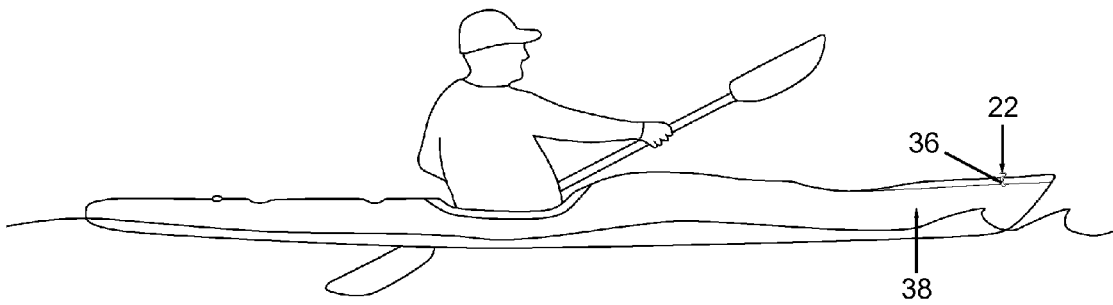


FIG. 14

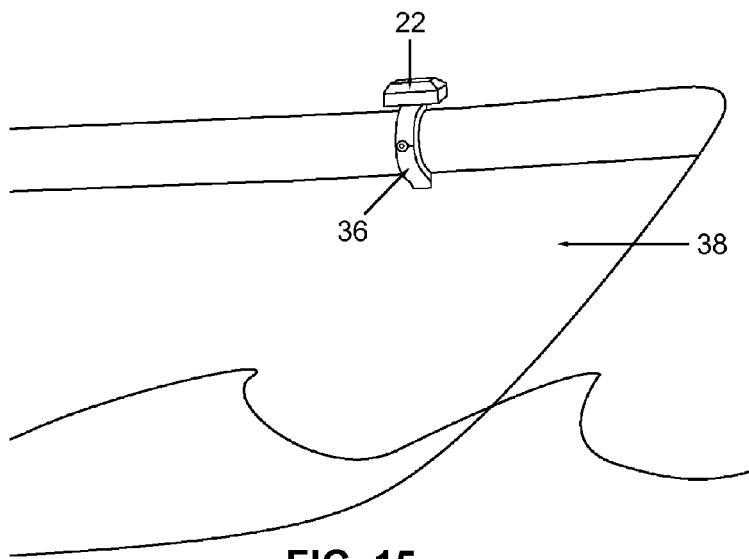


FIG. 15

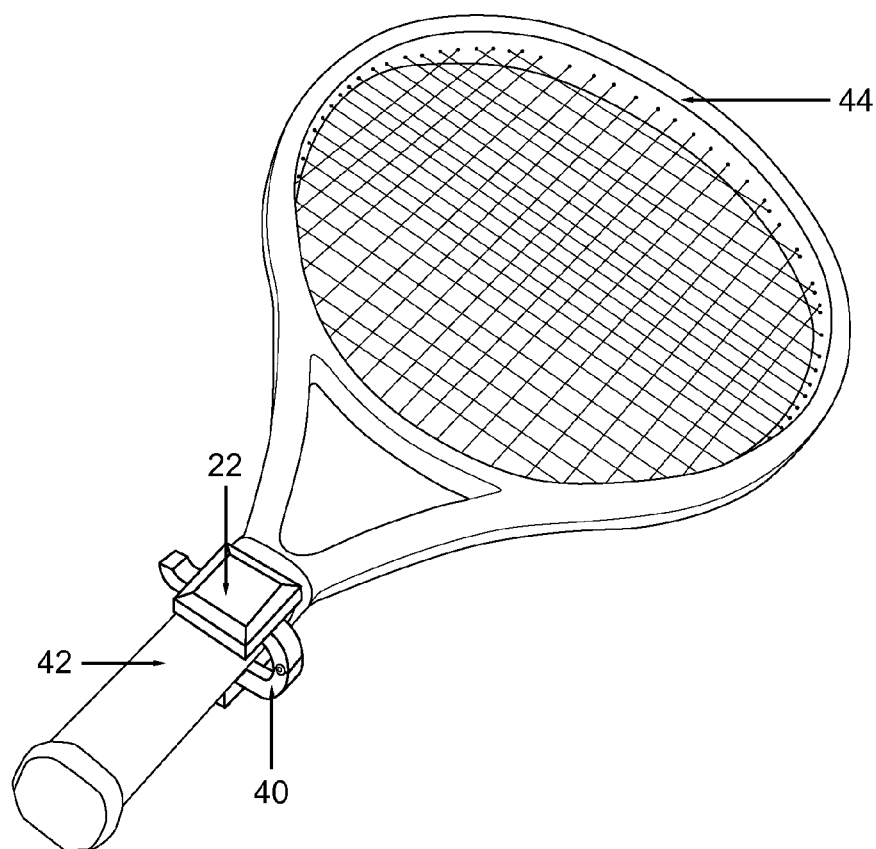


FIG. 16

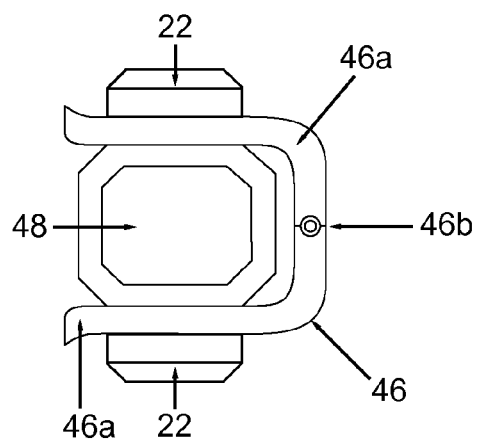


FIG. 17

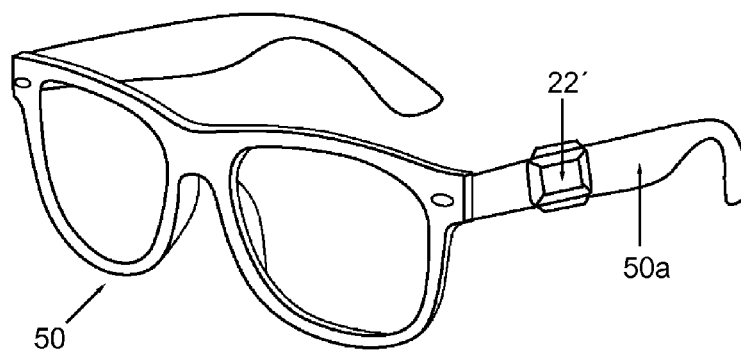


FIG. 18

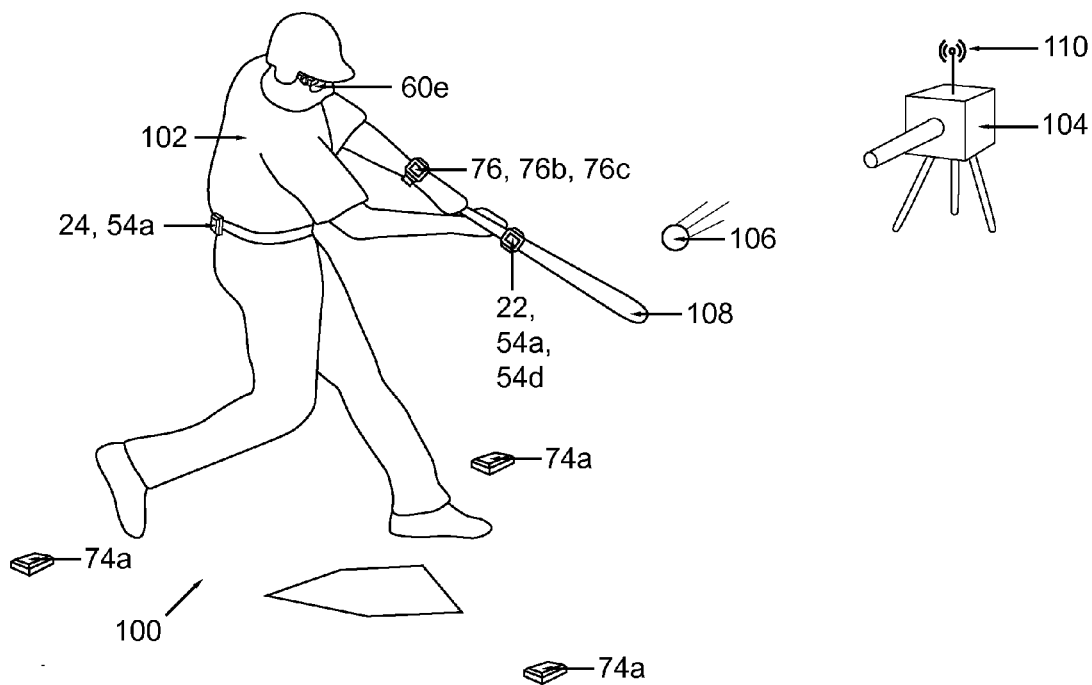


FIG. 19

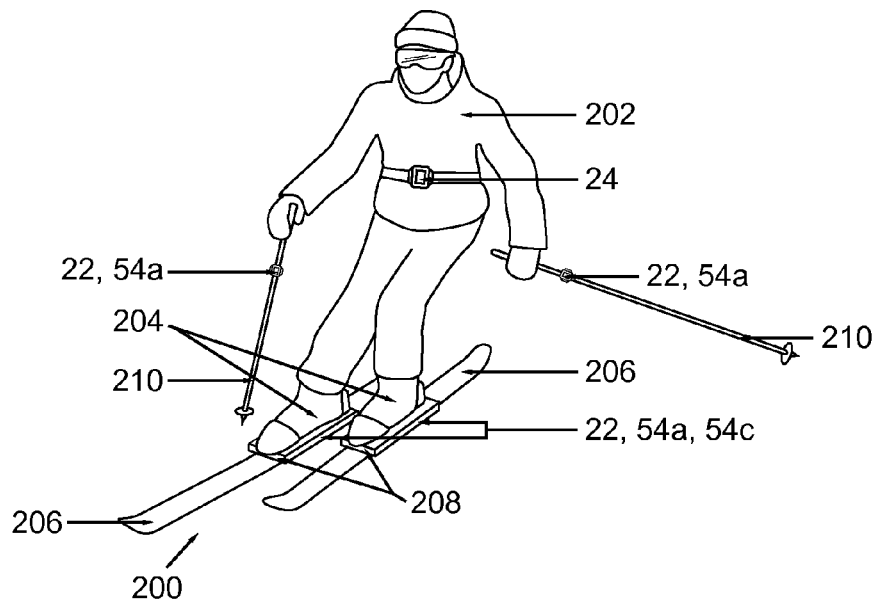


FIG. 20

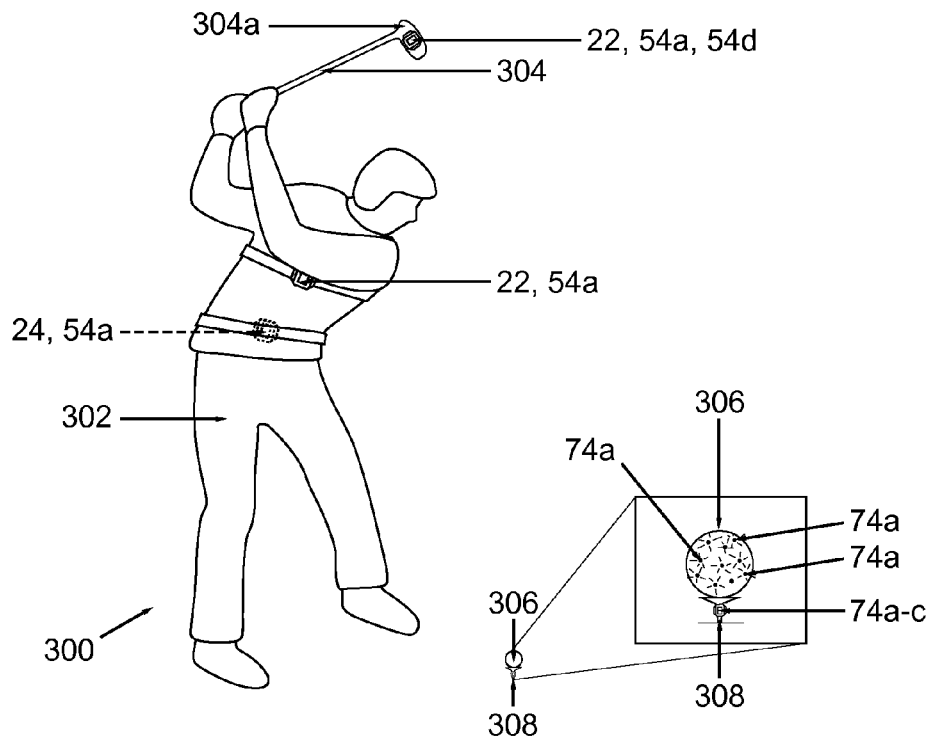


FIG. 21A

FIG. 21B

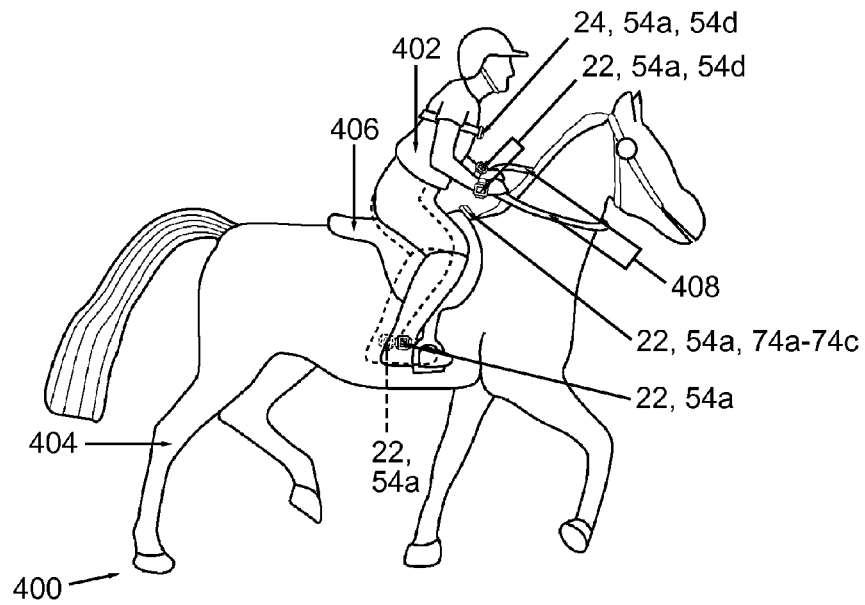


FIG. 22

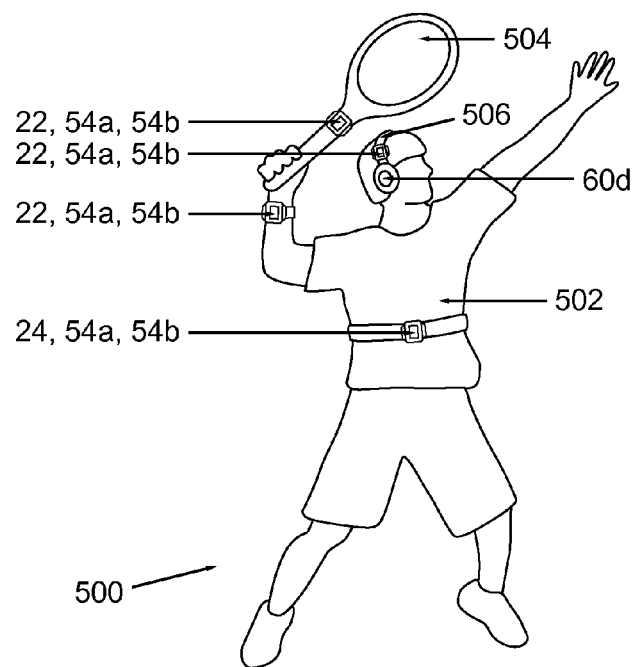


FIG. 23

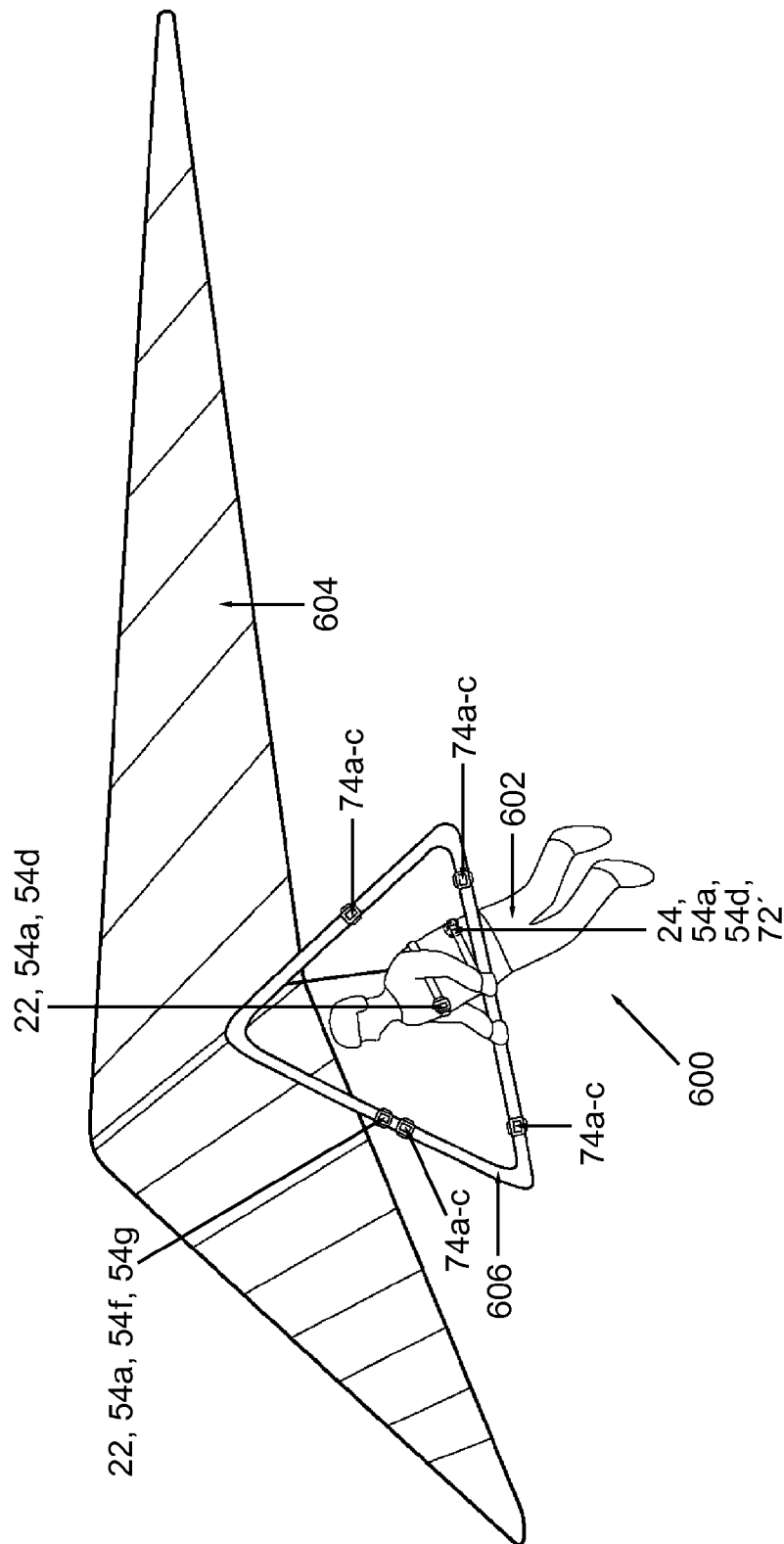


FIG. 24

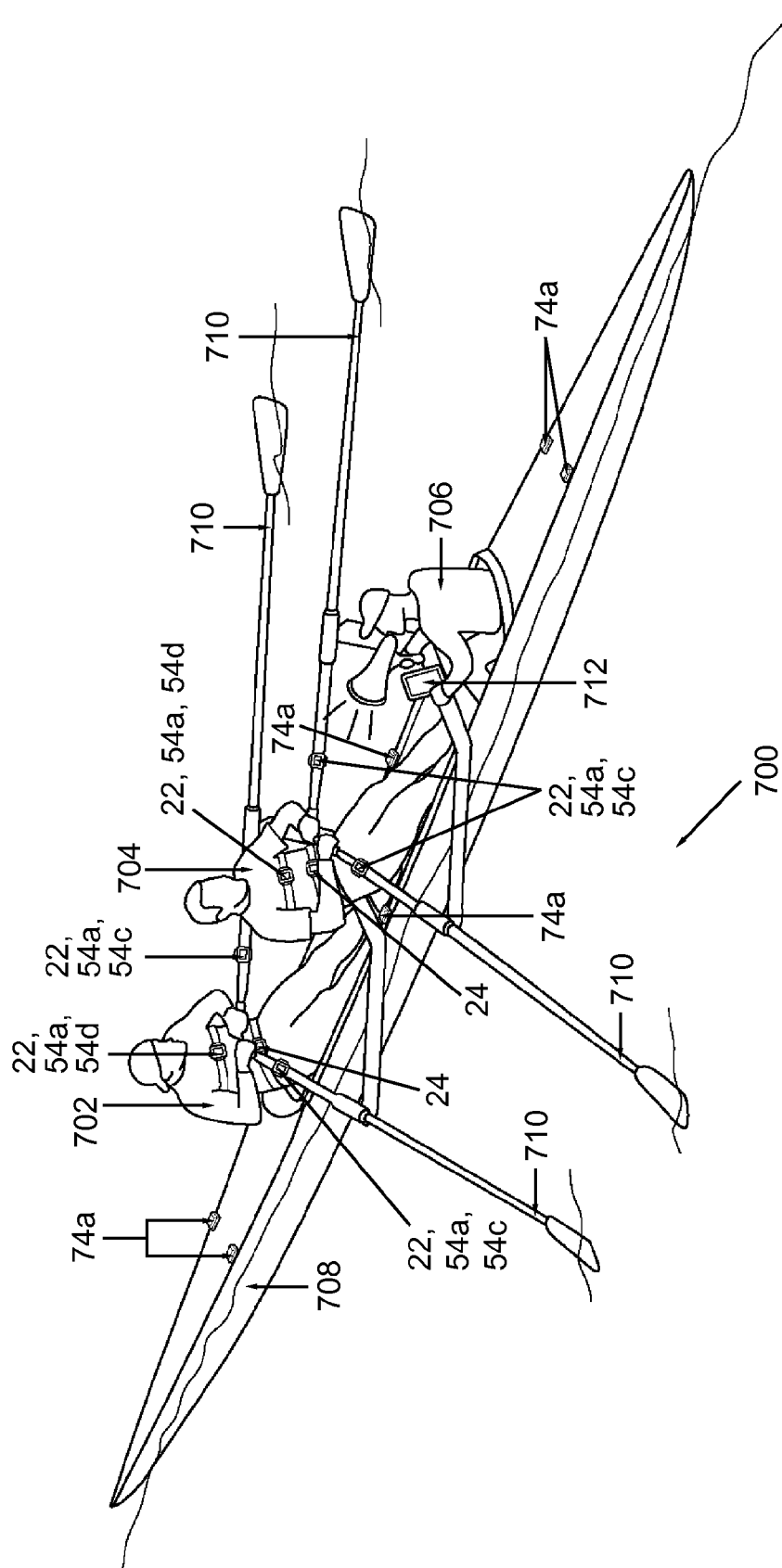


FIG. 25

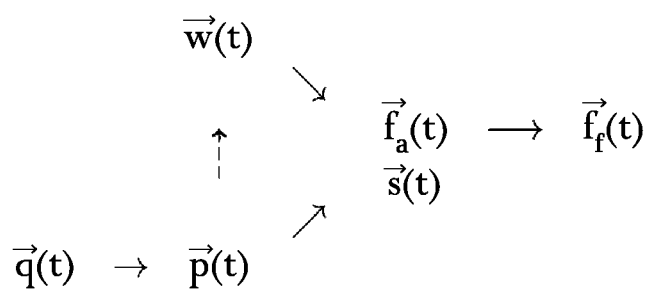


FIG. 26

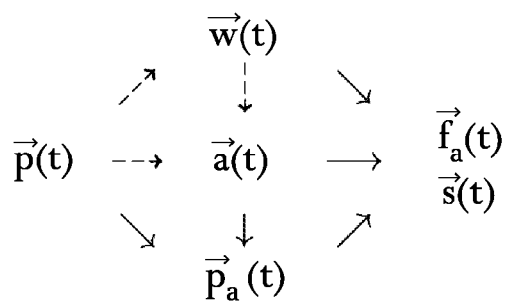


FIG. 27

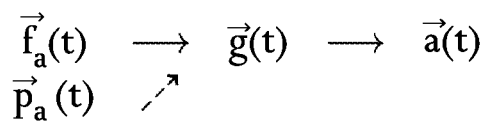
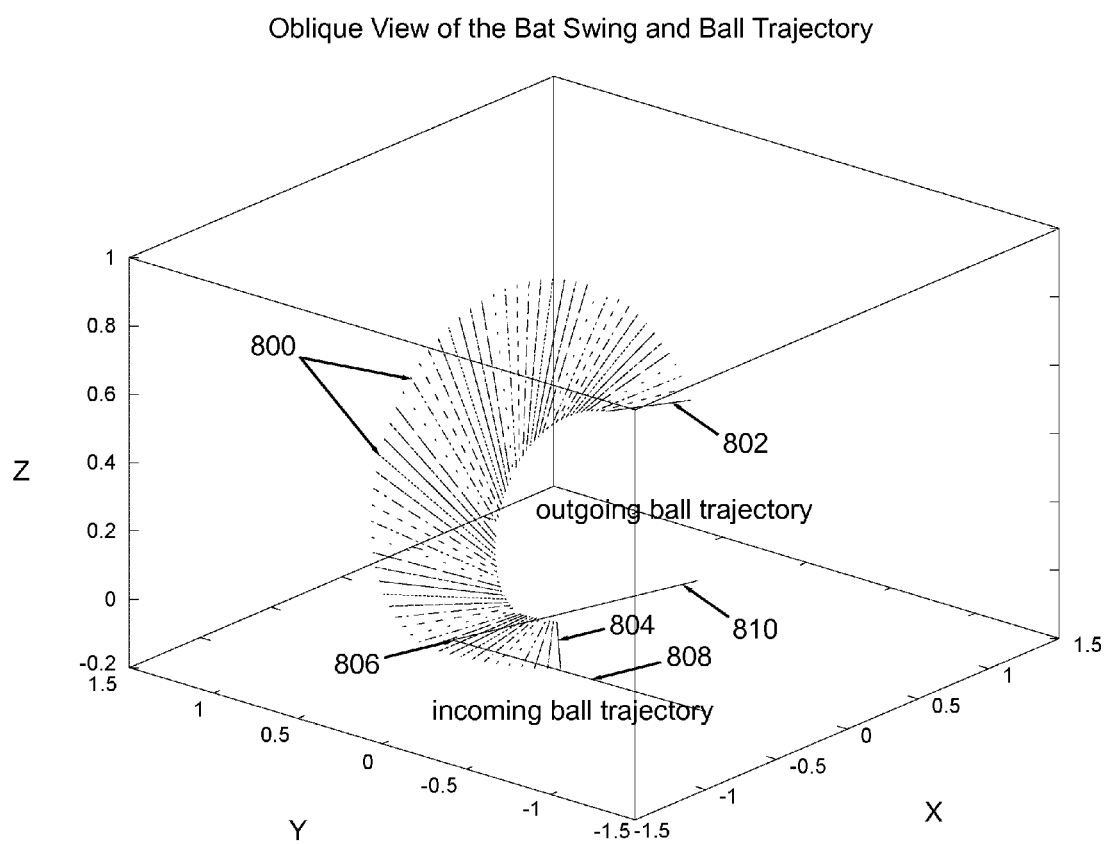
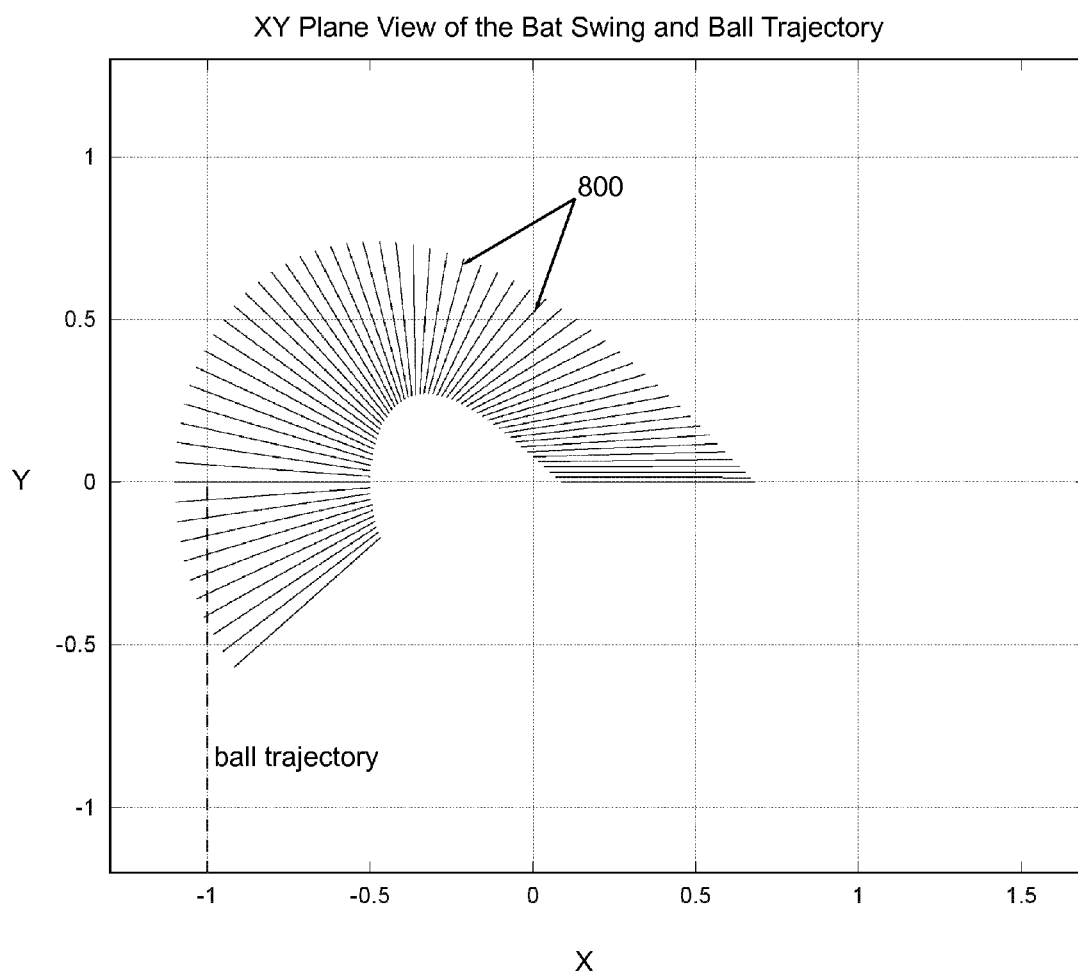
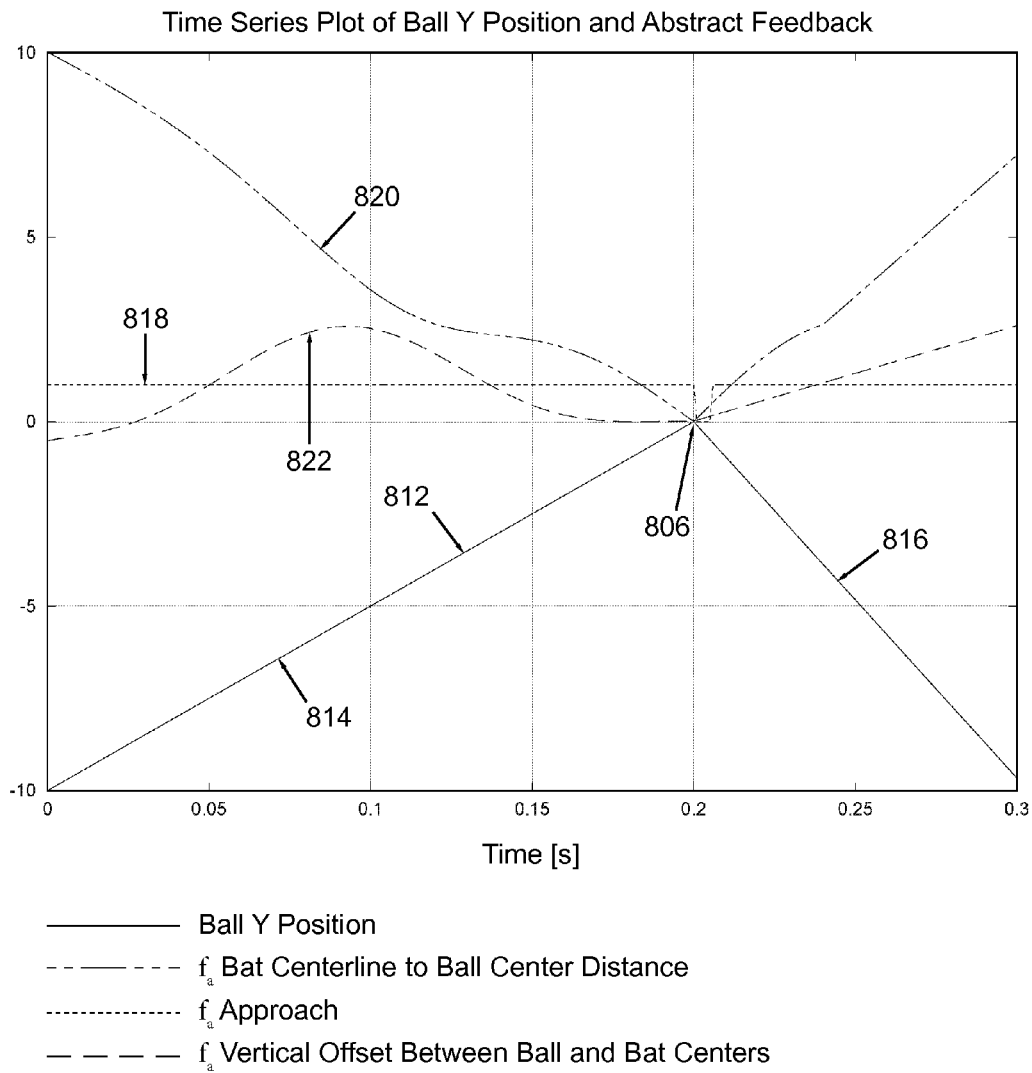


FIG. 28

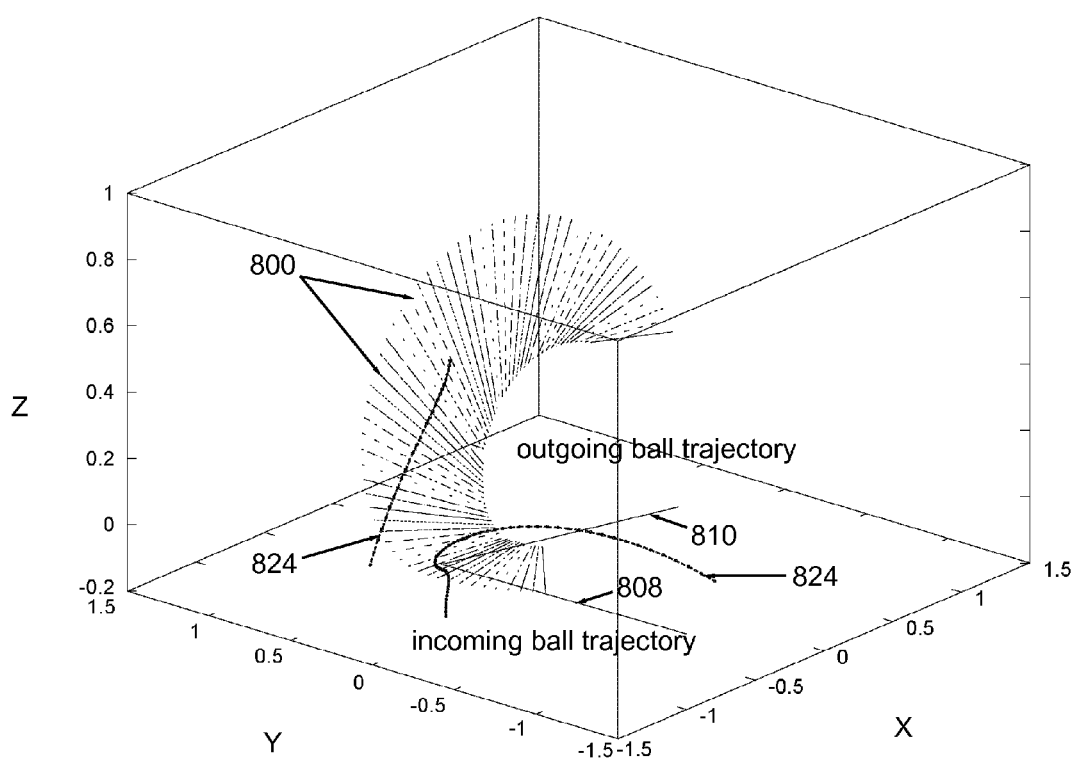
**FIG. 29**

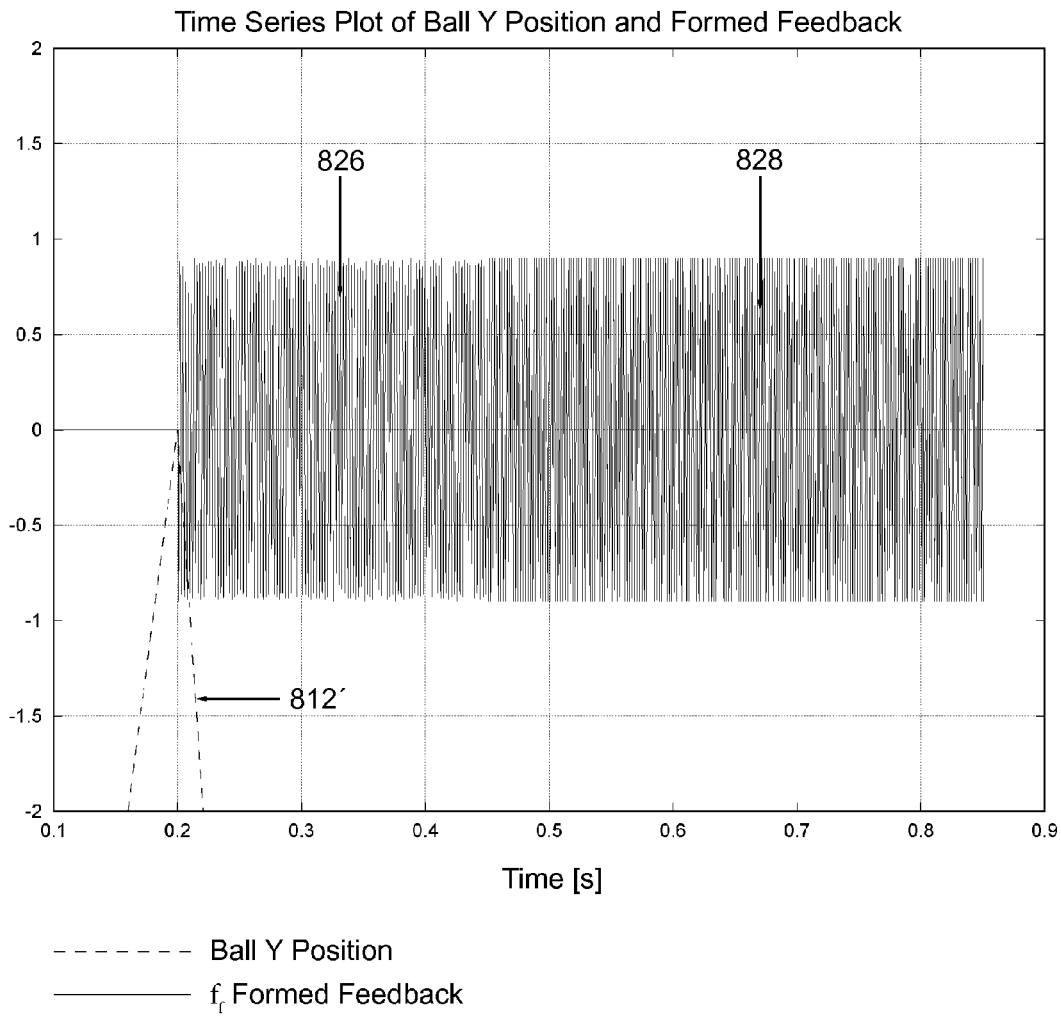
**FIG. 30**

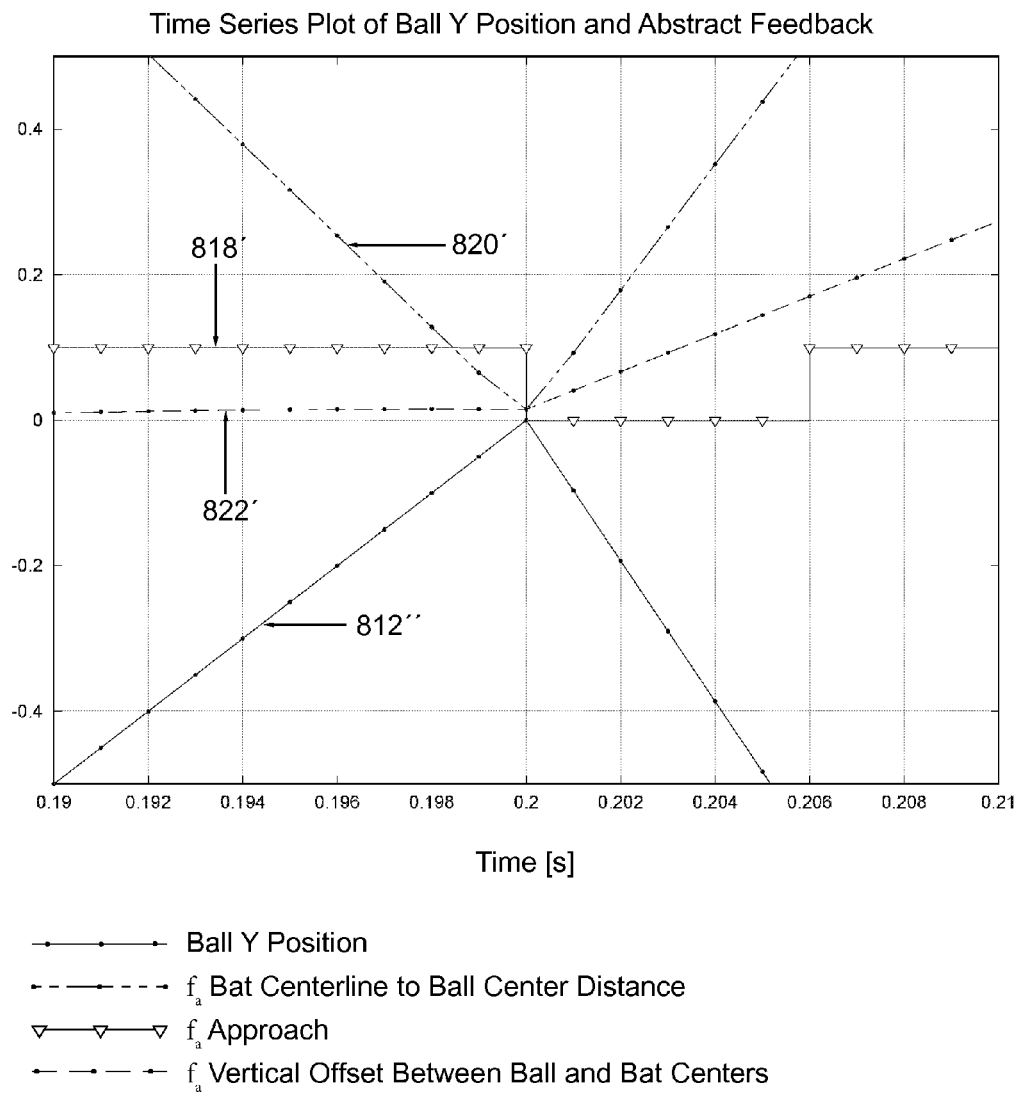
**FIG. 31**

**FIG. 32**

Oblique View of the Bat Swing, Ball Trajectory and the Feedback Agreeing Form

**FIG. 33**

**FIG. 34**

**FIG. 35**

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MOVEMENT ASSESSMENT APPARATUS AND A METHOD FOR PROVIDING BIOFEEDBACK USING THE SAME

CROSS-REFERENCE TO RELATED APPLICATIONS

Not Applicable.

STATEMENT REGARDING FEDERALLY SPONSORED RESEARCH OR DEVELOPMENT

Not Applicable.

NAMES OF THE PARTIES TO A JOINT RESEARCH AGREEMENT

Not Applicable.

INCORPORATION BY REFERENCE OF MATERIAL SUBMITTED ON A COMPACT DISK

Not Applicable.

BACKGROUND OF THE INVENTION

1. Field of the Invention

The invention generally relates to a movement assessment apparatus. More particularly, the invention relates to a movement assessment apparatus configured to provide biofeedback to a user regarding one or more bodily movements executed by the user, and a method for providing biofeedback using the same.

2. Background

Training for a sporting activity or dance performance usually requires going through the same motion repeatedly. Typically, a coach or trainer first tells the trainee what to do, and then observes the motion and corrects mistakes. Particularly, in movements performed quickly, the coach explains the mistakes after the trainee performs the activity. This may take the form of showing a video of the trainee performing the activity, and then pointing out the errors. Seeing the mistakes after the fact is not as effective as getting instantaneous feedback while performing the activity. Still more effective is the feedback conveying not only at what point the mistake is made, but also letting the trainee know the magnitude of the error.

Therefore, what is needed is a movement assessment apparatus that is capable of providing biofeedback to a user regarding one or more bodily movements executed by the user. Moreover, what is needed is a method for providing biofeedback to a user regarding one or more bodily movements executed thereby that can be used to enhance the user's performance of a particular activity. Furthermore, a motion assessment apparatus is needed that can be effectively utilized during a plurality of different movement activities performed by a user, such as during the performance of various sports.

BRIEF SUMMARY OF EMBODIMENTS OF THE INVENTION

Accordingly, the present invention is directed to a movement assessment apparatus and method for providing biofeedback using the same that substantially obviates one or more problems resulting from the limitations and deficiencies of the related art.

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In accordance with one or more embodiments of the present invention, there is provided a movement assessment apparatus configured to provide biofeedback to a user regarding one or more bodily movements executed by the user. The movement assessment apparatus includes: at least one sensing device, the at least one sensing device comprising one or more sensors for detecting the motion of a body portion of a user and outputting one or more signals that are generated based upon the motion of the body portion of the user, the at least one sensing device further comprising attachment means for attaching the at least one sensing device to the body portion of the user; a data processing device operatively coupled to the at least one sensing device, the data processing device configured to receive the one or more signals that are output by the one or more sensors of the at least one sensing device, and to determine a movement path and/or baseline velocity profile of the body portion of the user using the one or more signals, the data processing device further configured to compare the movement path and/or the velocity profile determined for the body portion of the user to a respective baseline movement path and/or velocity profile, and to determine how closely the movement path and/or the velocity profile determined for the body portion of the user conforms to the respective baseline movement path and/or baseline velocity profile, the data processing device additionally configured to generate a sensory output signal based upon the conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile; and a sensory output device operatively coupled to the data processing device, the sensory output device configured to receive the sensory output signal from the data processing device, to generate at least one of a visual indicator, an audible indicator, and a tactile indicator that is based upon the sensory output signal, and to output the at least one of the visual indicator, the audible indicator, and the tactile indicator to the user in order to provide biofeedback as to conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile.

In a further embodiment of the present invention, the one or more sensors of the at least one sensing device comprise at least one of: (i) an accelerometer, (ii) a gyroscope, and a geomagnetic sensor.

In yet a further embodiment, the at least one sensing device comprises a plurality of sensing devices, a first of the plurality of sensing devices configured to be attached to a limb of the user, and a second of the plurality of sensing devices configured to be attached to a first torso location of the user.

In still a further embodiment, the plurality of sensing devices further includes a third sensing device configured to be attached to a head of the user.

In yet a further embodiment, the plurality of sensing devices additionally includes a fourth sensing device configured to be attached to a second torso location of the user.

In still a further embodiment, the attachment means of the at least one sensing device comprises a resilient band for attaching the at least one sensing device to one of a limb of the user, a torso of the user, and a head of the user.

In yet a further embodiment, the data processing device comprises a microprocessor.

In still a further embodiment, the movement assessment apparatus further comprises a band for attaching the data processing device to a torso of the user.

In yet a further embodiment, the sensory output device comprises an audio headset configured to be worn on a head of the user, and wherein the audio headset is configured to generate the audible indicator that provides biofeedback as to

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conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile.

In still a further embodiment, the audible indicator generated by the audio headset is in the form of a pleasant sound when the movement path of the user substantially conforms to the baseline movement path, and wherein the audible indicator generated by the audio headset is in the form of an unpleasant sound when the movement path of the user does not generally conform to the baseline movement path.

In yet a further embodiment, the audible indicator generated by the audio headset becomes increasingly more unpleasant to the user as the movement path of the user deviates to a greater degree from the baseline movement path.

In still a further embodiment, the at least one sensing device further comprises one or more additional sensors for detecting at least one of: (i) a position of the user, (ii) a body parameter of the user, and (iii) an environmental parameter.

In yet a further embodiment, the one or more additional sensors of the at least one sensing device comprise at least one of: (i) a global positioning system sensor for detecting a position of the user, (ii) a body oxygenation sensor for detecting an oxygen level or oxygen saturation level of the user, (iii) a body temperature sensor for detecting a body temperature of the user, (iv) an ambient temperature sensor for detecting a temperature of an environment in which the user is disposed, and (v) a humidity sensor for detecting a humidity level of the environment in which the user is disposed.

In still a further embodiment, the sensory output device comprises a light emitting device configured to be worn by the user, and wherein the light emitting device is configured to generate the visual indicator that provides biofeedback as to conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile.

In yet a further embodiment, the sensory output device comprises a vibratory device configured to be worn by the user, and wherein the vibratory device is configured to generate the tactile indicator that provides biofeedback as to conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile.

In still a further embodiment, one or more parameters of the baseline movement path and/or the baseline velocity profile are adjustable so as to accommodate at least one of: (i) a plurality of different activities performed by the user, (ii) a skill level of the user with respect to a particular activity, (iii) a particular movement style of the user, and (iv) physical limits of the user.

In yet a further embodiment, the movement assessment apparatus further comprises means for adjusting a sensitivity of the biofeedback provided by the apparatus so as to accommodate users of different skill levels.

In still a further embodiment, the movement assessment apparatus is configured to provide real-time biofeedback to the user.

In accordance with one or more other embodiments of the present invention, there is provided a method for providing biofeedback to a user regarding one or more bodily movements executed by the user. The method comprising the steps of: (i) providing a movement assessment apparatus configured to be worn by a user, the movement assessment apparatus including: at least one sensing device, the at least one sensing device comprising one or more sensors for detecting the motion of a body portion of a user and outputting one or more signals that are generated based upon the motion of the body portion of the user, the at least one sensing device further

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comprising attachment means for attaching the at least one sensing device to the body portion of the user; a data processing device operatively coupled to the at least one sensing device, the data processing device configured to receive the one or more signals that are output by the one or more sensors of the at least one sensing device, and to determine a movement path and/or velocity profile of the body portion of the user using the one or more signals, the data processing device further configured to compare the movement path and/or the velocity profile determined for the body portion of the user to a respective baseline movement path and/or velocity profile, and to determine how closely the movement path and/or the velocity profile determined for the body portion of the user conforms to the respective baseline movement path and/or baseline velocity profile, the data processing device additionally configured to generate a sensory output signal based upon the conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile; and a sensory output device operatively coupled to the data processing device, the sensory output device configured to receive the sensory output signal from the data processing device, to generate at least one of a visual indicator, an audible indicator, and a tactile indicator that is based upon the sensory output signal, and to output the at least one of the visual indicator, the audible indicator, and the tactile indicator to the user in order to provide biofeedback as to conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile; (ii) outfitting a user with the movement assessment apparatus, which includes attaching the attachment means of the at least one sensing device to a body portion of the user; (iii) instructing the user to perform an activity where the user displaces the body portion with the at least one sensing device attached thereto; (iv) detecting, by utilizing the at least one sensing device, the motion of the body portion of the user and outputting one or more signals that are generated based upon the motion of the body portion of the user; (v) receiving, at the data processing device, the one or more signals that are output by the one or more sensors of the at least one sensing device; (vi) determining, by using the data processing device, a movement path and/or velocity profile of the body portion of the user using the one or more signals; (vii) comparing, by using the data processing device, the movement path and/or the velocity profile determined for the body portion of the user to a respective baseline movement path and/or velocity profile; (viii) determining, by using the data processing device, how closely the movement path and/or the velocity profile determined for the body portion of the user conforms to the respective baseline movement path and/or baseline velocity profile; (ix) generating, by using the data processing device, a sensory output signal based upon the conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or velocity profile; (x) receiving, at the sensory output device, the sensory output signal from the data processing device; (xi) generating, by using the sensory output device, at least one of a visual indicator, an audible indicator, and a tactile indicator that is based upon the sensory output signal; and (xii) outputting the at least one of the visual indicator, the audible indicator, and the tactile indicator from the sensory output device to the user in order to provide quasi-instantaneous, real-time biofeedback as to conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile.

In a further embodiment of the present invention, the method further comprises the step of guiding the body portion of the user as the user displaces the body portion during the

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performance of the activity. In this embodiment, the instructor guides the body portion of the user during the displacement of the body portion along an intended path of movement.

In accordance with yet one or more other embodiments of the present invention, there is provided a movement and performance assessment apparatus configured to provide biofeedback to a user regarding one or more bodily movements executed by the user. The movement and performance assessment apparatus includes: at least one sensing device, the at least one sensing device comprising one or more first sensors for detecting the motion of a body portion of a user and outputting one or more first signals that are generated based upon the motion of the body portion of the user, the at least one sensing device further comprising one or more second sensors for detecting at least one of: (i) a position of the user, (ii) a body parameter of the user, and (iii) an environmental parameter, the one or more second sensors outputting one or more second signals, and the at least one sensing device additionally comprising attachment means for attaching the at least one sensing device to the body portion of the user; a data processing device operatively coupled to the at least one sensing device, the data processing device configured to receive the one or more first signals that are output by the one or more first sensors of the at least one sensing device, to receive the one or more second signals that are output by the one or more second sensors of the at least one sensing device, and to determine a movement path and/or velocity profile of the body portion of the user using the one or more first signals, the data processing device further configured to compare the movement path and/or the velocity profile determined for the body portion of the user to a respective baseline movement path and/or velocity profile, and to determine how closely the movement path and/or the velocity profile determined for the body portion of the user conforms to the respective baseline movement path and/or baseline velocity profile, the data processing device additionally configured to generate a sensory output signal based upon the conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile; and a sensory output device operatively coupled to the data processing device, the sensory output device configured to receive the sensory output signal from the data processing device, to generate at least one of a visual indicator, an audible indicator, and a tactile indicator that is based upon the sensory output signal, and to output the at least one of the visual indicator, the audible indicator, and the tactile indicator to the user in order to provide biofeedback as to conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile.

In a further embodiment of the present invention, the one or more second sensors of the at least one sensing device comprise at least one of: (i) a global positioning system sensor for detecting a position of the user, (ii) a body oxygenation sensor for detecting an oxygen level or oxygen saturation level of the user, (iii) a body temperature sensor for detecting a body temperature of the user, (iv) an ambient temperature sensor for detecting a temperature of an environment in which the user is disposed, and (v) a humidity sensor for detecting a humidity level of the environment in which the user is disposed.

In yet a further embodiment, the movement and performance assessment apparatus further comprises a remote computing device operatively coupled to the movement and performance assessment apparatus, the remote computing device comprising a data storage device for storing data

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acquired by the movement and performance assessment apparatus, the remote computing device further comprising a data processing device for analyzing the data acquired by the movement and performance assessment apparatus.

In still a further embodiment, the movement and performance assessment apparatus further comprises a counting device configured to measure a number of repetitions of an activity performed by the user, the counting device operatively coupled to the data processing device so that the measured number of repetitions are capable of being used in a performance analysis of the user.

It is to be understood that the foregoing general description and the following detailed description of the present invention are merely exemplary and explanatory in nature. As such, the foregoing general description and the following detailed description of the invention should not be construed to limit the scope of the appended claims in any sense.

BRIEF DESCRIPTION OF THE SEVERAL VIEWS OF THE DRAWINGS

The invention will now be described, by way of example, with reference to the accompanying drawings, in which:

FIG. 1 is a diagrammatic front perspective view of a user or subject outfitted with a movement assessment system, according to one embodiment of the invention;

FIG. 2 is a diagrammatic rear perspective view of a user or subject outfitted with a movement assessment system, according to the embodiment of the invention in FIG. 1;

FIG. 3 is a schematic block diagram of pertinent electrical components of an illustrative sensor unit of the movement assessment system, according to an embodiment of the invention;

FIG. 4 is a schematic block diagram of pertinent electrical components of an illustrative central control unit of the movement assessment system, according to an embodiment of the invention;

FIG. 5 illustrates various forms in which wireless data interface(s) of the exemplary movement assessment system may be embodied, according to an embodiment of the invention;

FIG. 6 illustrates various forms in which wired data interface(s) of the exemplary movement assessment system may be embodied, according to an embodiment of the invention;

FIG. 7 illustrates various forms in which sensor(s) of the exemplary movement assessment system may be embodied, according to an embodiment of the invention;

FIG. 8 illustrates various forms in which sensory output device(s) of the exemplary movement assessment system may be embodied, according to an embodiment of the invention;

FIG. 9 illustrates various forms in which motion tracker reference source(s) of the exemplary movement assessment system may be embodied, according to an embodiment of the invention;

FIG. 10 illustrates various forms in which a user interface of the exemplary movement assessment system may be embodied, according to an embodiment of the invention;

FIG. 11 is a diagrammatic perspective view of first exemplary attachment means for the sensor unit of the movement assessment system, according to one embodiment of the invention;

FIG. 12 is a diagrammatic perspective view of second exemplary attachment means for the sensor unit of the movement assessment system, according to another embodiment of the invention;

FIG. 13 is a diagrammatic perspective view of third exemplary attachment means for the sensor unit of the movement assessment system, according to yet another embodiment of the invention;

FIG. 14 is a diagrammatic perspective of a sensor unit of the movement assessment system attached to a boat using fourth exemplary attachment means, according to still another embodiment of the invention;

FIG. 15 is an enlarged perspective view of a portion of FIG. 14 illustrating in greater detail the manner in which the fourth exemplary attachment means of the sensor unit is coupled to the top rim of the boat;

FIG. 16 is a diagrammatic perspective view of fifth exemplary attachment means for the sensor unit of the movement assessment system, according to yet another embodiment of the invention, wherein the fifth exemplary attachment means is used to attach the sensor unit to a handle of a tennis racket;

FIG. 17 is an end view illustrating in greater detail the manner in which the fifth exemplary attachment means is used to attach the sensor unit to the handle of the tennis racket;

FIG. 18 is a diagrammatic perspective view of the sensor unit of the movement assessment system attached to an eyeglass frame, according to yet another embodiment of the invention;

FIG. 19 is a diagrammatic perspective view of a first exemplary scenario wherein the movement assessment system described herein is being used to assess the athletic performance of a baseball player;

FIG. 20 is a diagrammatic perspective view of a second exemplary scenario wherein the movement assessment system described herein is being used to assess the athletic performance of a skier;

FIG. 21A is a diagrammatic perspective view of a third exemplary scenario wherein the movement assessment system described herein is being used to assess the athletic performance of a golfer;

FIG. 21B is an enlarged perspective view of the golf ball and tee in FIG. 21A, which further illustrates the details of the motion tracker reference sources on the golf ball and tee;

FIG. 22 is a diagrammatic perspective view of a fourth exemplary scenario wherein the movement assessment system described herein is being used to assess the athletic performance of a horseback rider;

FIG. 23 is a diagrammatic perspective view of a fifth exemplary scenario wherein the movement assessment system described herein is being used to assess the athletic performance of a tennis player;

FIG. 24 is a diagrammatic perspective view of a sixth exemplary scenario wherein the movement assessment system described herein is being used to assess the athletic performance of a handglider;

FIG. 25 is a diagrammatic perspective view of a seventh exemplary scenario wherein the movement assessment system described herein is being used to assess the athletic performance of a rowing team;

FIG. 26 is a flow diagram of an exemplary motion-based biofeedback calculation process that is carried out by the motion assessment apparatus and system described herein;

FIG. 27 is a flow diagram illustrating an exemplary abstract feedback signal generation process that is carried out by the motion assessment apparatus and system described herein;

FIG. 28 is a flow diagram illustrating an exemplary adaptation signal generation process that is carried out by the motion assessment apparatus and system described herein;

FIG. 29 is a three-dimensional (3D) plot illustrating a bat swing and ball trajectory generated by the exemplary movement assessment software code described herein;

FIG. 30 is a plot illustrating a bat swing and ball trajectory in the Y-Z plane as generated by the exemplary movement assessment software code described herein;

FIG. 31 is a plot illustrating a bat swing and ball trajectory in the X-Y plane as generated by the exemplary movement assessment software code described herein;

FIG. 32 is a time series plot illustrating ball Y position and abstract feedback as generated by the exemplary movement assessment software code described herein;

FIG. 33 is a three-dimensional (3D) plot illustrating bat swing, ball trajectory, and the feedback agreeing form as generated by the exemplary movement assessment software code described herein;

FIG. 34 is a time series plot illustrating ball Y position and formed feedback as generated by the exemplary movement assessment software code described herein; and

FIG. 35 is an enlarged view of a portion of FIG. 32, which illustrates the ball Y position and abstract feedback around the time of contact as generated by the exemplary movement assessment software code described herein.

Throughout the figures, the same parts are always denoted using the same reference characters so that, as a general rule, they will only be described once.

DETAILED DESCRIPTION OF EMBODIMENTS OF THE INVENTION

Initially, with reference to FIGS. 1 and 2, an illustrative embodiment of a movement assessment system 10 for providing biofeedback to a user 12 regarding one or more bodily movements executed by the user is shown. In FIG. 1, it can be seen that a user 12 may be outfitted with a plurality of different sensor band devices 14, 16, 18, 20 for detecting the motion of the user 12. In the illustrative embodiment, a user 12 is provided with a first sensor band device 14 on a wrist of his or her right arm, a second sensor band device 16 around his or her waist, a third sensor band device 18 around his or her chest, and a fourth sensor band device 20 around his or her head. In the illustrative embodiment, the second sensor band device 16 around the waist of the user 12 comprises a central control unit 24 (see FIG. 2), while the sensor band devices 14, 18, and 20 each comprise sensor units 22. In the illustrated embodiment, each of the sensor units 22 is operatively coupled to the central control unit 24 by wireless means, such as Bluetooth, or another suitable type of personal area network wireless means. However, in other embodiments, each of the sensor units 22 may be operatively coupled to the central control unit 24 by a wired connection.

In the illustrated embodiment of FIGS. 1 and 2, each of the sensor units 22 is coupled to the respective body portion of the user 12 by a band. In FIG. 11, the first sensor band device 14, which attaches to the wrist of the user 12, is illustrated in more detail. As illustrated in this figure, the first sensor band device 14 generally comprises a sensor unit 22 attached to an elastic band 26. The band 26 is resilient so that it is capable of being stretched to accommodate the hand of the user 12, and then, fitted in place on the wrist of the user 12. The band 26 can be formed from any suitable stretchable fabric, such as neoprene, spandex, and elastane. Alternatively, the band 26 could be formed from a generally non-stretchable fabric, and be provided with latching means or clasp means for allowing the band 26 to be split into two portions (e.g., the band 26 could be provided with a snap-type latching device).

As illustrated in FIGS. 11-18, it is also possible to attach the sensor units 22 to the body portions of the user 12 using other suitable attachment means. For example, as shown in FIG. 12, the sensor unit 22 may be attached to a surface 30

(e.g., the skin or clothing item of the user 12 using adhesive backing means 28. The adhesive backing means 28 may comprise a removable backing member that is removed just prior to the sensor unit 22 being attached to a user 12 or object. Also, in some embodiments, the adhesive backing means 28 may comprise a form of double-sided bonding tape that is capable of securely attaching the sensor unit 22 to the user 22 or another object. As another example, referring to FIG. 13, the sensor unit 22 may be attached to a surface 32 (e.g., a metallic surface 32) using a magnetic attachment means (the magnetic flux lines 34 are shown in FIG. 13 to diagrammatically illustrate the magnetic attractive force between the magnetic attachment means of the sensor unit 22 and the metallic surface 32).

In FIGS. 14-17, sensor units 22 attached by various clamping devices 36, 40, 46 are illustrated. In FIGS. 14 and 15, the sensor unit 22 is attached to the edge of a hull 38 of a boat, such as a rowboat, canoe, or kayak, by a C-shaped clamping device 36. Turning to FIGS. 16 and 17, it can be seen that two sensor units 22 are attached to opposed sides of a handle 42 of a tennis racket 44 by a clamping device 40. FIG. 17 illustrates an end view of a sensor unit 22 attached to a tennis racket handle 42 with handle end 48 by a hinged C-clamp device 46. Similarly, the C-clamp device 46 may be used to attach sensor unit 22 to other elongate objects, such as the shaft of a golf club. As shown in FIG. 17, the clamping portions 46a of the C-clamp device 46 pivot about a hinge portion 46b.

Another mounting arrangement for a sensor unit 22' is shown in FIG. 18. In this figure, the sensor unit 22' is mounted to an eyeglass frame 50. In particular, the sensor unit 22' is attached to the temple portion 50a of the eyeglass frame 50. The sensor unit 22' is preferably more compact, and smaller in size, than the sensor unit 22 so that it can be easily attached to the eyeglass frame 50 without resulting in the deformation of the eyeglass frame 50 due to excessive weight applied thereto.

Hereafter, exemplary embodiments of the present invention will be described with reference to block diagrams that diagrammatically illustrate the architecture of various components of the movement assessment system 10. With respect to these diagrammatic illustrations, it is to be understood that the connecting lines shown in the block diagram(s) included herein are intended to represent functional relationships and/or operational couplings between the various components. The compound conjunction "and/or" is used throughout this disclosure to mean one or the other, or both. For example, when a data processing device is said to be configured to determine a movement path and/or velocity profile, this is equivalent to stating that the data processing device is configured to determine a movement path, a velocity profile, or both a movement path and a velocity profile.

Now, with reference to FIG. 3, an exemplary sensor unit 22 that may be utilized in conjunction with the embodiments described herein will be described in detail. As shown in FIG. 3, the sensor unit 22 generally comprises a processing circuit 52, one or more sensors 54 that are operatively coupled to the processing circuit 52, volatile memory 58 operatively coupled to the processing circuit 52 for storing data during the processing thereof, and a power supply and conditioner 56 operatively coupled to each of the electrical components 52, 54, 58. The processing circuit 52 may comprise a microprocessor or other suitable processing means. The power supply and conditioner 56 regulates the power that is delivered to the electrical components 52, 54, 58 by modifying the level and characteristics thereof (e.g., by regulating the voltage delivered from the power supply 66, 68, 70 by adjusting the voltage level and characteristics in accordance with the specific needs of the electrical components 52, 54, 58). Referring again to

FIG. 3, it can be seen that the power supply or power source for the sensor unit 22 may be in the form of a battery 66 disposed within the sensor unit 22 itself, a wireless power receiver 68 operatively coupled to a remote wireless power transmitter, and/or a wired power input 70 (e.g., an electrical wire or wires connecting the sensor unit 22 to the power supply in the central control unit 24). As shown in FIG. 3, no matter which one or combination of the power supplies 66, 68, 70 is used in the sensor unit 22, the power supplies 66, 68, 70 are all operatively connected to the power supply and conditioner 56 so that the power delivered thereby can be conditioned prior to being transmitted to the electrical loads (e.g., electrical components 52, 54, 58) in the sensor unit 22. If a wireless power receiver 68 is utilized as the power supply for the sensor unit 22, a wireless power transmitter 80' may be located in the central control unit 24 of the movement assessment system 10. Also, in addition to volatile memory 58, the sensor unit 22 also may have non-volatile memory 72 in the form of a data storage device, such as one or more compact hard drives, flash drives, memory cards, memory sticks, or any combination thereof.

Also, as shown in FIG. 3, the sensor unit 22 may comprise one or more wireless data interfaces 62 for electrically coupling the sensor unit 22 to other devices, such as a central control unit 24. In particular, with reference to FIG. 5, the one or more wireless data interfaces 62 may comprise a Bluetooth device 62a for operating as part of a personal area network ("PAN"), a Wi-Fi device 62b for operating as part of a wireless local area network ("WLAN"), and/or a proprietary wireless interface device 62c that utilizes a proprietary communications protocol. It is to be understood that the sensor unit 22 may comprise one, two, or all three of these data interface devices 62a, 62b, 62c depending on the needs of the particular movement assessment system 10 in which they are being utilized.

Referring again to FIG. 3, the sensor unit 22 also may comprise one or more wired data interfaces 64 for electrically coupling the sensor unit 22 to other devices, such as a central control unit 24, by hard wiring (e.g., an electrical wire or cable). Specifically, with reference to FIG. 6, the one or more wired data interfaces 64 may comprise a universal serial bus ("USB") port 64a for accommodating a USB cable between devices (e.g., between devices 22, 24) and/or a proprietary data port 64b for accommodating a proprietary cable between devices (e.g., between devices 22, 24). It is to be understood that the sensor unit 22 may comprise one or both of these wired data interfaces 64 depending on the needs of the particular movement assessment system 10 in which they are being employed.

As described above in conjunction with FIG. 3, the sensor unit 22 comprises one or more sensors 54 for sensing one or more measurable quantities associated with a subject or user (e.g., an athlete) or an object (e.g., a boat, a golf ball, a handglider, etc.). With reference to FIG. 7, the one or more sensors 54 in the sensor unit 22 may comprise an inertial sensor 54a for measuring motion, a magnetometer-type sensor 54b for measuring the orientation of the user or object relative to the Earth's magnetic field, a load sensor 54c for measuring the force and/or moments exerted on a particular user or object, a motion tracking sensor 54d for measuring the motion of a user or object, an optical sensor 54e for measuring the motion of a user or object using a reference light source, an air pressure sensor 54f for measuring the ambient air pressure or pressure inside a particular enclosure, a global positioning system ("GPS") sensor 54g for measuring the location or position of a user or object anywhere on or near the Earth using satellite technology, a body oxygenation sensor 54h for detecting an

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oxygen level or oxygen saturation level of a subject or user (e.g., athlete), a body temperature sensor **54i** for detecting a body temperature of the user, an ambient temperature sensor **54j** for detecting a temperature of an indoor or outdoor environment in which the user is disposed, and/or a humidity sensor **54k** for detecting a humidity level of the indoor or outdoor environment in which the user is disposed. It is to be understood that the sensor unit **22** may comprise any number or all of these sensors **54a**, **54b**, **54c**, **54d**, **54e**, **54f**, **54g**, **54h**, **54i**, **54j**, **54k** depending on the needs of the particular movement assessment system **10** in which they are being employed.

In one or more further embodiments, the one or more inertial sensors **54a** for measuring motion may comprise one or more of the following: (i) an accelerometer, (ii) a gyroscope, (iii) a magnetometer, and (iv) a geomagnetic sensor. Also, the one or more inertial sensors **54a** may include a plurality of each of the following sensor types in order to measure motion in multiple directions (e.g., three accelerometers to measure acceleration in three (3) dimensional space). The data processing device (e.g., the processing circuit **52'**, which may include a microprocessor) of the central control unit **24** and/or the data processing device (e.g., the processing circuit **52**, which may include a microprocessor) of the sensor unit **22** may utilize the output signals of the one or more inertial sensors **54a** to determine a movement path and/or velocity profile of the body portion of the user while he or she is performing a particular activity (i.e., the data processing device may determine a movement path, a velocity profile, or both a movement path and a velocity profile of the body portion of the user). The data processing device (e.g., the processing circuit **52'**, which may include a microprocessor) of the central control unit **24** and/or the data processing device (e.g., the processing circuit **52**, which may include a microprocessor) of the sensor unit **22** is further configured to compare the movement path and/or the velocity profile determined for the body portion of the user to a respective baseline movement path and/or velocity profile (i.e., the data processing device may compare a movement path, a velocity profile, or both a movement path and a velocity profile of the body portion of the user to a respective baseline movement path or baseline velocity profile). The data processing device (e.g., the processing circuit **52'**, which may include a microprocessor) of the central control unit **24** and/or the data processing device (e.g., the processing circuit **52**, which may include a microprocessor) of the sensor unit **22** is further configured to determine how closely the movement path and/or the velocity profile determined for the body portion of the user conforms to the respective baseline movement path and/or baseline velocity profile (i.e., the data processing device may determine how closely a movement path, a velocity profile, or both a movement path and a velocity profile of the body portion of the user conforms to the respective baseline movement path or baseline velocity profile). Finally, the data processing device (e.g., the processing circuit **52'**, which may include a microprocessor) of the central control unit **24** and/or the data processing device (e.g., the processing circuit **52**, which may include a microprocessor) of the sensor unit **22** is configured to generate a sensory output signal based upon the conformity of the movement path and/or the velocity profile of the user to the respective baseline movement path and/or baseline velocity profile.

Also, in one or more further embodiments, the global positioning system ("GPS") sensor **54g** may be used to track the location of the activity that the user is performing. For example, if the user is a golfer, the global positioning system ("GPS") sensor **54g** may be used to determine the location of

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the golf course that the golfer is playing. That way, the user is not required to manually track the location of each of his or her activities, thereby streamlining the assessment of his or her performance.

In addition, in one or more further embodiments, the body parameters of the user and environmental conditions may be sensed by the sensors **54**, **54'**. For example, the temperature and humidity of the environment (e.g., outdoor or indoor environment) in which the user is performing the activity may be sensed by air temperature sensor **54j** and the humidity sensor **54k**, respectively, while the air pressure of the environment may be sensed by the air pressure sensor **54f**. For example, if the user is a golfer, the environmental sensors **54j**, **54k**, and **54f** may be used to assess the weather conditions that the golfer is experiencing during his or her round of golf. Of course, if the weather conditions are adverse, this could significantly affect the performance of the golfer during his or her round of golf. Advantageously, the inclusion of the environmental sensors **54j**, **54k**, and **54f** allow the movement and performance assessment apparatus and system to automatically track the performance of the user based upon specific weather conditions. The body parameters of the user who is executing the activity may also be correlated with his or her performance. For example, the body oxygenation sensor **54h** and the body temperature sensor **54i** may be used to monitor the physiological state of the user while he or she is performing the activity being monitored. Based upon the physiological parameters measured by the sensors **54h**, **54i**, the movement and performance assessment system may advantageously help a user determine if his or her performance is being adversely affected by his or her uncomfortable physiological state. For example, if the body temperature sensor **54i** indicates that the user is too cold or too hot, the movement and performance assessment system could output this result to the user so that a user's unsatisfactory performance of a particular activity could be correlated with the abnormal body temperature.

Next, with reference once again to FIG. 3, the sensor unit **22** also may comprise one or more sensory output devices **60** for providing sensory stimuli to a subject or user so as to enable the movement assessment system **10** to provide the subject or user with biofeedback regarding his or her movement. In particular, with reference to FIG. 8, the one or more sensory output devices **60** may comprise a thermal or heat-based sensor output device **60a** for delivering heat to the skin of a subject or user (i.e., a first type of tactile sensor output device), a vibratory sensory output device **60b** for delivering vibrations to the limb or torso of a subject (i.e., a second type of tactile sensor output device), a light-emitting sensor output device **60c** for providing a visual cue to a subject or user, an auditory sensory output device **60d** for delivering an audible cue to the subject or user, and/or a visual display sensor output device **60e** for providing a visual cue to a subject or user using an output display device. It is to be understood that the sensor unit **22** may comprise any number or all of these sensory output devices **60a**, **60b**, **60c**, **60d**, **60e** depending on the needs of the particular movement assessment system **10** in which they are being employed.

In one or more embodiments, the auditory sensory output device **60d** may comprise an audio headset that generates an audible cue in the form of a pleasant sound when the movement path and/or velocity profile of the user substantially conforms to the respective baseline movement path and/or baseline velocity profile (e.g., a sound with a frequency spectrum that lies within a comfortable range for the user, such as 2,000 Hertz or lower, or a sound having a comfortable decibel level for the user). In contrast, when the movement path

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and/or velocity profile of the user does not generally conform to the respective baseline movement path and/or baseline velocity profile, the audio headset generates an audible cue in the form of a unpleasant sound (e.g., a sound with a frequency spectrum that lies within an uncomfortable range for the user, such as between 2,000 Hertz and 4,000 Hertz, or a sound having a uncomfortable decibel level for the user, such as a sound over 100 decibels). In one or more other embodiments, the audible cue or sound generated by the audio headset becomes increasingly more unpleasant to the user as the movement path and/or velocity profile of the user deviates to a greater degree from the respective baseline movement path and/or baseline velocity profile (e.g., the decibel level of the sound gradually increases or the frequency level increases from a comfortable range to an uncomfortable range).

Referring again to FIG. 3, the sensor unit 22 also may comprise one or more motion tracker reference sources 74 for providing a point or frame of reference for any motion tracking sensors 54d that are used in conjunction with the movement assessment system 10. Specifically, as shown in FIG. 9, the one or more motion tracker reference sources 74 may comprise a motion tracker reference light source 74a for emitting light therefrom, a motion tracker reference magnetic signal 74b for generating a magnetic force and/or creating a magnetic field, and/or a motion tracker reference ultrasonic signal 74c for emitting an ultrasonic signal therefrom. It is to be understood that the sensor unit 22 may comprise one, two, or all three of these motion tracker reference sources 74a, 74b, 74c depending on the needs of the particular movement assessment system 10 in which they are being employed.

Turning again to FIG. 3, the sensor unit 22 also may comprise a user interface 76 for allowing the subject or user to interact with the sensor unit 22 by controlling the settings thereof, etc. In particular, as shown in FIG. 10, the user interface 76 may comprise one or more buttons 76a that can be pressed by a user thereof, a display 76b (i.e., visual display) that allows the user to view, for example, settings that can be adjusted on the sensor unit 22, and/or a touch input 76c that enables a user to interact with the sensor unit 22 by inputting commands directly on the display (e.g., the touch input 76c allows the user to make selections and change settings directly on the screen of the sensor unit 22). It is to be understood that the user interface 76 of the sensor unit 22 may comprise one, two, or all three of these means of input 76a, 76b, 76c depending on the needs of the particular movement assessment system 10 in which they are being employed.

Next, with reference to FIG. 4, an exemplary central control unit 24 that may be utilized in conjunction with the embodiments described herein will be described in detail. The central control unit 24 operates as the central hub of the movement assessment system 10. As such, one or more satellite sensor units 22 may operatively communicate with the central control unit 24 using either wired or wireless means. As shown in FIG. 4, the central control unit 24 comprises, inter alia, a processing circuit 52', volatile memory 58' operatively coupled to the processing circuit 52' for storing data during the processing thereof, and a power supply and conditioner 56' operatively coupled to each of the electrical components 52', 58'. As described above for the sensor unit 22, the processing circuit 52' may comprise a microprocessor or other suitable processing means. Also, as described above for the sensor unit 22, the power supply and conditioner 56' regulates the power that is delivered to the electrical components 52', 58' by modifying the level and characteristics thereof (e.g., by regulating the voltage delivered from the power supply 66', 68', 70' by adjusting the voltage level and characteristics in accordance with the specific needs of the

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electrical components 52', 58'). Referring again to FIG. 4, it can be seen that the power supply or power source for the central control unit 24 may be in the form of a battery 66' disposed within the central control unit 24 itself, a wireless power receiver 68' operatively coupled to a remote wireless power transmitter, and/or a wired power input 70' (e.g., an electrical wire or wires connecting the central control unit 24 to an external power supply, such as a building electrical outlet or receptacle). For example, in some embodiments, the central control unit 24 could be provided with a rechargeable battery 66' and a battery charger configured to connect to the wired power input 70' for charging the rechargeable battery 66' when required. As shown in FIG. 4, no matter which one or combination of the power supplies 66', 68', 70' is used in the central control unit 24, the power supplies 66', 68', 70' are all operatively connected to the power supply and conditioner 56' so that the power delivered thereby can be conditioned prior to being transmitted to the electrical loads (e.g., electrical components 52', 58') in the central control unit 24. If a wireless power receiver 68' is utilized as the power supply for the central control unit 24, the central control unit 24 may be utilized in conjunction with an external wireless power transmitter. Also, in addition to volatile memory 58', the central control unit 24 also may have non-volatile memory 72' in the form of a data storage device, such as one or more compact hard drives, flash drives, memory cards, memory sticks, or any combination thereof.

Also, as shown in FIG. 4, the central control unit 24 may comprise one or more wireless data interfaces 62' for electrically coupling the central control unit 24 to other devices, such as one or more satellite sensor units 22 or a remote computing device. As explained above for the sensor unit 22, the one or more wireless data interfaces 62' may include a Bluetooth device 62a, a Wi-Fi device 62b, and/or a proprietary wireless interface device 62c that utilizes a proprietary communications protocol (refer to FIG. 5). Turning again to FIG. 4, the central control unit 24 may comprise one or more wired data interfaces 64' for electrically coupling the central control unit 24 to other devices, such as one or more satellite sensor units 22, by hard wiring (e.g., an electrical wire or cable), or to a remote computing device. Similar to that described above for the sensor unit 22, the one or more wired data interfaces 64' may include a universal serial bus ("USB") port 64a and/or a proprietary data port 64b (see FIG. 6).

In a further embodiment, the movement and performance assessment system may comprise a remote computing device operatively coupled to the movement and performance assessment apparatus by means of the one or more wireless data interfaces 62' and/or the one or more wired data interfaces 64'. The remote computing device may include a data storage device for storing data acquired by the movement and performance assessment apparatus, and a data processing device (e.g., a microprocessor or other processing means) for analyzing the data acquired by the movement and performance assessment apparatus. The remote computing device may be in the form of a laptop computing device, a tablet, a smartphone, or another type of remote computing device. The remote computing device may be provided with one or more software applications or software programs loaded thereon for tracking the performance of the user during the performance of his or her activities and/or to analyze the results of his or her performance after the activity has been concluded (i.e., the software applications or software programs may enable an "after-the-fact" analysis to be performed on the collected performance data). Advantageously, the post-activity analysis performed by the remote computing device complements the real-time biofeedback provided by the con-

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trol unit **24** and/or the sensor unit **22**. In one or more further embodiments, the remote computing device may be in form of central computing device (i.e., server) for collecting all of the performance data in a central location. The central computing device may comprise a cloud-based computing device for storing the performance data at a remote site.

Also, in one or more further embodiments, the central control unit **24** and/or the sensor unit **22** of the movement and performance assessment system may comprise a counting device configured to measure a number of repetitions of an activity performed by the user. The counting device may be operatively coupled to the data processing device (e.g., the processing circuit **52'**, which may include a microprocessor) of the central control unit **24** and/or the data processing device (e.g., the processing circuit **52**, which may include a microprocessor) of the sensor unit **22** so that the measured number of repetitions are capable of being used in a performance analysis of the user.

In addition, referring again to FIG. 4, the central control unit **24** may include one or more sensors **54'** for sensing one or more measurable quantities associated with a subject or user (e.g., an athlete) or an object (e.g., a boat, a golf ball, a handglider, etc.). As explained above for the sensor unit **22**, the one or more sensors **54'** in the central control unit **24** may comprise an inertial sensor **54a**, a magnetometer-type sensor **54b**, a load sensor **54c**, a motion tracking sensor **54d**, an optical sensor **54e**, an air pressure sensor **54f**, a global positioning system ("GPS") sensor **54g**, a body oxygenation sensor **54h**, a body temperature sensor **54i**, an ambient temperature sensor **54j**, and/or a humidity sensor **54k** (refer to FIG. 7). With reference again to FIG. 4, the central control unit **24** also may comprise one or more sensory output devices **60'** for providing sensory stimuli to a subject or user so as to enable the movement assessment system **10** to provide the subject or user with biofeedback regarding his or her movement. As described above for the sensor unit **22**, the one or more sensory output devices **60'** may comprise a thermal or heat-based sensor output device **60a**, a vibratory sensory output device **60b**, a light-emitting sensor output device **60c**, an auditory sensory output device **60d**, and/or a visual display sensor output device **60e** (see FIG. 8).

As illustrated in the block diagram of FIG. 4, the central control unit **24** also may comprise one or more motion tracker reference sources **74'** for providing a point or frame of reference for any motion tracking sensors **54d** that are used in conjunction with the movement assessment system **10**. As explained above for the sensor unit **22**, the one or more motion tracker reference sources **74'** may comprise a motion tracker reference light source **74a**, a motion tracker reference magnetic signal **74b**, and/or a motion tracker reference ultrasonic signal **74c** (refer to FIG. 9). In FIG. 4, it can be seen that the central control unit **24** additionally may comprise a user interface **76'** for allowing the subject or user to interact with the central control unit **24** by controlling the settings thereof, etc. Similar to that described above in conjunction with the sensor unit **22**, user interface **76'** of the central control unit **24** may comprise one or more buttons **76a**, a display **76b** (i.e., visual display), and/or a touch input **76c** (see FIG. 10).

Turning once again to FIG. 4, it can be seen that the central control unit **24** may further include a wired peripheral interface **78'** for operatively coupling the central control unit **24** to an external peripheral device, such as a pair of audio headphones or a wearable display device (e.g., an optical head-mounted display (OHMD), such as Google® Glass™).

Next, an illustrative manner in which the data processing device (e.g., the processing circuit **52, 52'**, which may include a microprocessor) of the movement assessment apparatus or

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system **10** performs the motion-based biofeedback calculations will be explained in detail. In particular, this calculation procedure will describe the manner in which a movement path of the body portion of the user is determined using one or more signals from the at least one sensing device. This calculation procedure will additionally describe the manner in which the movement path determined for the body portion of the user is compared to a baseline movement path, as well as the manner in which it is determined how closely the movement path determined for the body portion of the user conforms to the baseline movement path. Similarly, this calculation procedure will explain the manner in which the velocity profile determined for the body portion of the user is compared to a baseline velocity profile, as well as the manner in which it is determined how closely the velocity profile determined for the body portion of the user conforms to the baseline velocity profile. In one or more embodiments, the velocity profile is the velocity expressed as a function of a scalar parameter representing position along the path of motion. As such, in this case, both the velocity and position must be determined. Also, in one or more embodiments, the term "parameter" shall mean a scalar or a vector parameter. The term "component" shall mean a single scalar component of a vector parameter, or a scalar parameter itself.

In some embodiments, the executed motion is treated in its most general sense, without limiting to any particular set of its parameters, or any particular subsequent transformation of those parameters into a different representation. For example, just measuring the air velocity at the end of a baseball bat is potentially useful by itself to estimate the aerodynamic drag on the bat. The air velocity is relative to the motion of surrounding air, and only available at a point (i.e., thus, in this case, it is not necessary to determine the overall angular velocity of the rigid body of the bat).

It is to be understood that the aforescribed functionality and calculation processes of the movement assessment apparatus or system **10** can be carried out by the data processing device (e.g., **52, 52'**) utilizing software, hardware, or a combination of both hardware and software. For example, the data processing device (e.g., **52, 52'**) can be specially programmed to carry out the functionality described hereinafter. In one embodiment of the invention, the computer program instructions necessary to carry out this functionality may be loaded directly onto an internal data storage device (e.g., **58, 58', 72, 72'**) of the data processing device (e.g., **52, 52'**) and subsequently executed by the microprocessor of the data processing device (e.g., **52, 52'**). Alternatively, these computer program instructions could be stored on a portable computer-readable medium (e.g., a flash drive, a memory stick, etc.), and then subsequently loaded onto the data processing device (e.g., **52, 52'**) such that the instructions can be executed thereby. In other embodiments, these computer program instructions could be embodied in the hardware of the data processing device (e.g., **52, 52'**), rather than in the software thereof. It is also possible for the computer program instructions to be embodied in a combination of both the hardware and the software. Also, in the disclosure, when a reference is made to a data processing device or computing device that is "configured to", "arranged to" and/or "configured and arranged to" perform a specific function (e.g., a data processing device or computing device configured and arranged to perform a specific function), it is to be understood that, in one or more embodiments of the invention, this means that the data processing device or computing device is specially programmed to carry out the particular function (e.g., the data processing device or computing device being specially programmed to perform a specific function).

The motion-based biofeedback calculation process can be generally described by the flow diagram in FIG. 26. In this figure, $\vec{w}(t)$ represents the reference motion, which can be pre-computed, or derived in real time from the executed motion, or both pre-computed and derived in real time from the executed motion. Also, referring again to this figure, $\vec{p}(t)$ represents the real-time capture of the executed motion, which is obtained from the raw motion data $\vec{q}(t)$. The abstract feedback signal $\vec{f}_a(t)$ in FIG. 26 is generated from both the real-time capture of the motion data $\vec{p}(t)$ and the reference motion $\vec{w}(t)$, while the formed feedback signal $\vec{f}_f(t)$ is obtained from the abstract feedback signal by the process of feedback forming, a provision of the feedback by actuating the formed feedback. In FIG. 26, the selection signal $\vec{s}(t)$ is used for automatic selection of the appropriate reference motion, abstract feedback and formed feedback based on the activity being performed. The notations utilized in FIG. 26 (i.e., $\vec{w}(t)$, $\vec{p}(t)$, $\vec{q}(t)$, etc.) represent that each of these functions comprises a vector-valued function of time t . An arrow indicates that the pointed-to quantity is also a function of the originating quantity, e.g. $\vec{q}(t) \rightarrow \vec{p}(t)$ implies $\vec{p}(t, \vec{q}(t))$: \vec{p} is a function of both time and $\vec{q}(t)$. A dashed arrow indicates that such relationship is optional.

In the illustrative embodiment, the objects being analyzed (e.g., the limbs of the user and various items of sporting equipment are generally modeled as rigid bodies. The movement assessment apparatus or system 10 utilizes rigid bodies as an approximation of more complex physical systems. For example, in the illustrative embodiment of the system 10, the following objects may be approximated as rigid bodies: (i) human body segments (e.g., forearm, thigh, head, etc.), (ii) rigid sports equipment (e.g., baseball bat, tennis racket, golf club), (iii) a handle of a hang glider, a top part of the saddle, etc. The sensor unit 22, through its attachment with a human body segment or the item of sports equipment, becomes integrated with the rigid body (i.e., the motion of the sensor unit 22 approximates that of the rigid body).

In the illustrative embodiment, the movement assessment apparatus or system 10 captures several important types of data. First, each of the sensor units 22, and each of the central control units 24 that include the sensor means, capture raw data, which comprises a time series of numeric values that represent the measured parameters of motion. The raw data is both time-discrete and value-discrete. That is, it is defined only at discrete points in time, and can take values from a finite set. The raw data collected by the sensing devices in the sensor units 22, and in the central control units 24, is also uncalibrated (i.e., the raw data does not have any of units of measurements associated with it). Prior to being utilized in the computations performed by the data processing device of the movement assessment apparatus or system 10, the raw data is converted into calibrated data with units of measurement associated therewith (e.g., velocity, position, etc.). In the illustrative embodiment, the calibration process may involve, inter alia, scaling, offset removal, linearization, filtering and sensor fusion. The sensor fusion combines inputs from multiple sensors to overcome their individual shortcomings. For example, output data from redundant sensing devices in a particular sensor unit 22 can be combined to arrive at a single output quantity (e.g., velocity, position, etc.). In the illustrative embodiment of the movement assessment apparatus or system 10, the vector-valued motion parameters may be defined in terms of a reference frame. That is, their values have given numerical values only in the context of such

a frame. Also, when there is more than one reference frame available, the motion parameters can be transformed between arbitrary frames. A reference frame, mathematically, is a coordinate system in space (i.e., it has an origin and cardinal directions). In the illustrative embodiment, a natural reference frame, which is denoted N , is rigidly attached to some point on the ground. Such a frame is only approximately inertial, as the earth rotates. It is to be understood that a reference frame itself can be fixed or variable in time. For example, a reference frame attached to a golf club moves and rotates as the club is swung. In addition, as mentioned above, the movement assessment apparatus or system 10 may additionally capture non-motion parameters, which do not pertain to the characterization of the motion itself. For example, ancillary parameters, which are useful in the further analysis of the data, include those that describe the state of the human, the environment, and other things that the human interacts with. For example, a hang-glider pilot's own body temperature, pulse and blood oxygenation can be captured, as well as the environmental temperature, air pressure and air speed.

The raw data utilized in the calculation process may be collected from a multitude of different sensors (e.g., sensor types 54a-54k described above), which may measure any of the following: (i) kinematic parameters of material points or rigid bodies, (ii) kinetic parameters at interfaces between elements of the biomechanical system, (iii) bulk thermodynamic and hydrodynamic parameters, (iv) optical parameters, (v) electrical parameters, and (vi) temporal parameters. The kinematic parameters of material points or rigid bodies may include: (a) position, linear velocity, linear acceleration, and (b) orientation, angular velocity, angular acceleration. The kinetic parameters at interfaces between elements of the biomechanical system may include: (a) contact force, and (b) contact pressure. The bulk thermodynamic and hydrodynamic parameters may include: (a) fluid pressure (e.g., blood pressure, atmospheric pressure), (b) fluid flow rate (e.g. breathing air flow, perspiration flow, blood flow), (c) fluid flow velocity (e.g., relative wind speed), (d) temperature (e.g. body temperature, surrounding air temperature), (e) partial pressure (e.g., partial pressure of CO_2 in expired air), and (f) thermal or optical power. The optical parameters may include: (a) radiant flux (e.g., radiant flux due to sunlight), and (b) optical absorption (e.g. in an optical gas analyzer, or in a photoplethysmographic blood oxygenation sensor). The electrical parameters may include: (a) electrophysiological potentials (e.g., electrocardiographic or electromyographic), and (b) generally considered impedance (e.g. chest impedance in a breathing sensor). Finally, the temporal parameters may include repetition rate (e.g. heart rate).

In the illustrative embodiment, the sensors 54, 54' (e.g., in sensor unit(s) 22 and central control unit(s) 24) output the raw data $\vec{q}(t)$ in the form of a time series of various components of parameters. That is, the raw data $\vec{q}(t)$ may be expressed as a vector function of time, defined only at discrete points t in time, and comprising n scalar parameters $q_1 \dots q_n$, each originating in a discrete sensing element:

$$\vec{q}(t) = (q_{r1}(t), q_{r2}(t), \dots, q_{rn}(t)) \quad (1)$$

The sensing element may be an integrated multi-channel device, inseparable into constituent sensing elements. Not all components may be defined for a given time point. For example, some signals may be sampled less often than the others. As an example, a sensor unit 22 comprising a tri-axial accelerometer may have captured the following data at 0.5 seconds from the start of capture:

$$\vec{q}_a(0.5 \text{ sec.}) = (312, 495, -1672) \quad (2)$$

The values in equation 2 above do not have a physical meaning until they are converted or transformed into calibrated

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data. After calibration, the data $\vec{p}(t)$ is given a meaning of the units of acceleration in a given reference frame.

In one or more embodiments, not all components measured by the sensors may be defined for a given time point. For example, some signals may be sampled less often than the others.

The calibrated, executed motion $\vec{p}(t)$ is obtained from raw data by using an appropriate combination of various processing methods. Generally, each of those methods can be expressed mathematically as a function (f) of all current and past raw data, as well as of time itself:

$$\vec{f}_c(t) = f(\{\forall_{t_\alpha < \tau < t} \vec{q}(\tau)\}, t) \quad (3)$$

The time history $\{\forall_{t_\alpha < \tau < t} \vec{q}(\tau)\}$ reads a set, for the time $t_\alpha < \tau < t$ since the start of the experiment (t_α) up to now (t), of the values of the executed raw motion \vec{q} . This formulation is general and affords useful flexibility in choosing a calibration process. In some calibration processes, the calibration functions may be time-variant (i.e., their effect on the signals they process may change over time). For example, a scaling and offset removal functions may be temperature-dependent to compensate for the temperature coefficient of the sensor. Faced with varying sensor temperature, the resulting calibration is time-variant. Also, in some calibration processes, the calibration functions may depend on the history of the data. For example, a temperature-dependent scaling and offset removal may also compensate for the thermal constants of the sensor if provided a history of prior values of the sensor's operating environment temperature.

The calibrated executed motion signal can be expressed as a sum of signals from contributing calibrations \vec{f}_{ci} , where i is the index of a contributing calibration:

$$\vec{p}(t) = \sum_i \vec{f}_{ci}(t) \quad (4)$$

A particular contributing calibration can provide just a subset of signals, the others being zero. In one or more embodiments, the following classes of calibration functions are utilized in order to convert the raw data into calibrated data: (i) demodulation, (ii) scaling, (iii) offset removal, (iv) linearization, (v) sensor fusion, (vi) filtering, and (vii) change of reference frame. Demodulation is the process of extracting the measured signal from a representation that was modulated in the transduction process itself. For a particular type of modulation employed in the sensor, the will be a matching demodulation scheme. Many modulation methods are known in telecommunications engineering. They can be utilized to facilitate the transduction process. The transduction itself may also have a property of producing a modulated raw signal that requires demodulation to obtain the direct representation of the measured quantity. For example, in a Doppler velocimeter, the sensor's output is a Doppler signal that must be frequency-demodulated to obtain the velocity signal. Scaling is the multiplication of a raw signal by a scaling constant that relates the physical units of measurement to arbitrary units of raw data. Offset removal is the subtraction of a reference value of a raw signal to relate the signal to a known reference quantity. Often the reference quantity represents a zero physical quantity. In such case, when the sensor output is at the reference value, it is known that the sensor is measuring a zero in terms of physical units of measure of some quantity. Linearization is the adjustment of a raw signal to correct for the non-linear relationship between the raw signal and the cali-

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brated value of the physical quantity intended to be measured by the sensor. The function representing this non-linear relationship may generally be a function of a number of raw or calibrated signals measured by other sensors, and it may be time-variant. Mathematically, such generalization is equivalent to sensor fusion. The choice of naming a given calibration process linearization, not sensor fusion, is arbitrary. It is only meant to indicate that the primary purpose of such fusion is to improve the linearity of a sensor (i.e., it is a hint to the engineer who uses the documentation of such a process). The Extended Kalman Filter is an example of a time-variant linearization function that may be utilized in one or more embodiments of the present invention. Sensor fusion is the combination of raw and/or calibrated data from multiple sensors to produce a calibrated parameter, often overcoming the shortcomings of individual sensors. The same set of raw sensor data can be processed in multiple ways to yield multiple calibrated parameters. The function representing a particular sensor fusion can be as general as necessary. Thus, both time-invariant and time-variant sensor fusion is possible, and both linear and non-linear functions may be employed. An example of a time-variant sensor fusion is a general form of the Kalman filter. Filtering is the adjustment of the frequency-domain properties of the signals. It can involve changing the frequency content and the phase of the signal undergoing filtering. The filtering may be, generally, time-variant (e.g., in a Kalman filter). The calibration function may also involve a change of reference frame. The vector-valued signal may have an associated frame of reference. The subsequent feedback generation may require the signals in a different reference frame. In an illustrative embodiment, the motion parameters or motion data may be transformed between different frames of reference. For example, in an exemplary scenario comprising a polo game, given a linear velocity ${}^R\vec{v}^M$ and the position ${}^R\vec{r}^M$ of a point on the mallet M in the reference frame attached to the rider's saddle R, and given the saddle's angular velocity in relation to ground, ${}^R\vec{\omega}^M$, we can obtain the linear velocity of the mallet in the natural (ground) reference frame as follows:

$${}^N\vec{v}^M = {}^R\vec{v}^M + {}^N\vec{\omega}^R \times {}^R\vec{r}^M \quad (5)$$

The availability of a signal in a given reference frame may be predicated by the chosen sensor arrangement. In the prior example, a motion tracker is tracking the mallet's position in reference to the saddle. An inertial reference mounted on the saddle then tracks the motion of the saddle in relation to an inertial frame. This second reference allows the transformation of the mallet position into an inertial reference frame.

It is to be understood that one mathematical process may have simultaneous functionality of multiple processing methods. The general form of Extended Kalman Filter can perform linearization, sensor fusion and filtering at once. Similarly, a finite-impulse-response (FIR1) or an infinite-impulse-response (IIR2) filter with matrix-valued coefficients, may perform filtering and sensor fusion at once when it acts on a vector-valued signal.

For example, suppose the data is referenced to the natural reference frame:

$${}^N\vec{p}(t) = (0.12, -0.91, -0.31) \frac{m}{s^2} \quad (6)$$

This data is discrete in time, thus the value of ${}^N\vec{p}(t)$ is only defined at discrete values of time t . Rather than being discrete in time, the data may alternatively be a continuous function of time, which is defined on a certain continuous time segment

$t_{\alpha} \leq t \leq t_{\omega}$. The continuous form is more succinct to write and alleviates the application-specific choices of numerical approximations. Also, the data may be mathematically transformed from a continuous form to discrete approximations (i.e., the data may be discretized). For example, integration may be approximated by summation according to a chosen numerical integration scheme.

Next, the reference or baseline motion utilized in conjunction with the embodiments of the present invention will be described. The components of the reference motion form a superset of the parameters of the executed motion:

$$\vec{w}(t) = (w_1(t), w_2(t), \dots, w_n(t)) \quad (7)$$

where for a certain possibly empty subset of indices j , the reference component j is the j -th component of the executed motion $w_j(t) = p_j(t)$.

For example, the reference signal can include a representation of the surface to which a motion should be constrained. Such a parameter is not present in the executed motion signal. Such a reference can be constant (e.g., a fixed terminal velocity of the piano key strived for when learning a particular expression level when playing a keyboard). The reference signal can be classified according to various aspects of its derivation.

First of all, the reference signal may be classified according to its temporal aspect. In particular, the reference signal can be based on an executed motion in the past or present, or on the limits of the motion feasible in the future. In some embodiments, the reference signal can be based on a captured prior performance. It may be the performance of the same subject, used to elicit improvement of performance, or to recover performance lost between seasons, or due to injury. Alternatively, the prior performance may belong to a high-level performer, to direct the subject's training towards such a standard.

In some embodiments, the executed motion underway could be the sole source of the feedback. The reference signal may be derived from any temporal subset of the motion. As one example, the distance from the starting point of the motion could be used to signal a sufficiently long draw of a bow. The reference is based on a very short past time segment of the motion. As another example, suppose an ideal swinging motion is to follow a particular surface, e.g. a plane or a cylinder of a given radius of curvature. A least-square-distance fit of the surface to the path of the motion executed thus far can be used to compute the normal distance of the currently executed position from the surface. The time-variant reference surface can be fixed—made invariant—after some criterion is met, e.g., after the motion has covered a set distance, or a set swing angle, or after reaching a set swing velocity. The reference signal may be derived from the segment of the motion between its start and the time a chosen criterion is met. The criterion may be null: then the entire motion up to now forms the reference.

In some embodiments, the reference signal can also be based on predicted future motion. The predicted future motion can take into account the performance limitations of the human musculoskeletal system. For example, suppose a given motion is to approach a target within a particular velocity range. In a particular configuration of the body segments, there are biological limits to the available torques and torque-change-rates. At a given time instant during the motion, it is possible to estimate how close to the biological limits the future motion must come to arrive at the target. It is thus possible to signal a-priori how close is the current motion is to precluding achievement of a correct result in the future.

Secondly, the reference signal may be classified according to its synthetic aspect. The degree of a reference signal's dependence on any captured motion can vary, from no dependence to a full dependence. The less dependent the reference signal is on a captured motion, the more synthetic it becomes. The degree of syntheticity may be defined using the information-theoretic concept of conditional entropy. Informally, the more entropy of the captured motion is preserved in the reference signal, the less synthetic it is. Formally, the larger the entropy of the captured motion \vec{p} conditioned on the reference motion \vec{w} , the more synthetic the reference motion is. The entropy of a signal, informally, is the amount of information carried by the signal. It is preconditioned on what is known a-priori. For example, considering the toss of a coin, the entropy of the resulting data is 1 bit, since the outcome is binary (one of two values). If the coin toss is performed with an unfair coin that is known to always give tails, the entropy is zero, since the outcome of the coin toss does not give any new information (i.e., one can always anticipate the result).

The non-synthetic reference is largely dependent on the captured motion. It preserves a relatively large amount of data from the motion. A representative example would be a captured motion that passes through a low-pass filter: it removes some frequency content from the reference, while passing the frequency components below the cut-off point unaltered. The dimensionality and units of measurement of the captured data are preserved, but some of the possible variability in the captured motion is lost.

The synthetic reference is a parametrized representation of the captured motion. The number of the parameters is much smaller than the number of values needed to represent the captured motion. The choice of the function(s) implementing such a reference is tailored to capture the aspects of the motion that are useful in subsequent generation of the feedback. For example, in training a particular curveball pitch, the reference may be the development in time of the ratio of energy between the rotational and linear motion of the ball—a scalar parameter. The full information about the motion of the ball, in comparison, has 6 degrees of freedom. The synthetic reference, in spite of being a parametrized representation of a motion, may still result in the same dimensionality and units of measurement of the resulting signal. In spite of it, the outputs of the synthetic reference are not able to accurately represent every possible captured motion.

Also, the selection of parameters constituting the reference motion signal can have a major impact on the usability and effectiveness of the feedback provided to the user. As such, one has to decide when to use parameter(s) from the captured motion versus a more synthetic parameter derived from those parameters. The functions presented below may also be applied in other areas of the processing chain, such as (i) during feedback forming, if the interaction of the nonlinearities of the synthetic parameter function with those of the abstract feedback function makes such choice preferable over the inclusion of the parameter in the reference; and (ii) during agreement (as described hereinafter), when the same synthetic parameter is to be compared between the reference and the executed motion.

The derivation of such synthetic parameters can be performed using various techniques. The techniques also can be combined. For example, given a three-dimensional (3D) vector parameter, one can compute the time derivative (velocity) of the vector, obtain the rotational component of the velocity, represent it with an Euler axis and an angle, project the Euler axis onto a two-dimensional (2D) plane, obtain the projection's magnitude and angle, and finally derive the angular

velocity from the angle. In one or more embodiments, the synthetic parameters may be derived using one or more of the following techniques: (i) projection, (ii) component selection, (iii) change of representation, (iv) time derivative and integrals, (v) energy and power, (vi) statistical measures, (vii) curve and surface fitting, (viii) domain transformations, (ix) event detection, (x) normalization, and (xi) truncation. Initially, with projection, a vector-valued parameter of a certain dimensionality m is projected onto a generalized lesser-dimensional surface, yielding a vector-valued parameter of a smaller dimensionality $1 \leq n < m$. When component selection is used, a subset of a vector's components may be selected for further use, for example, only the (x, y) components of an (x, y, z) vector.

Change of representation may also be used as the technique for deriving the synthetic parameters. The vector values may have multiple equivalent representations. Either a part or all of the alternate representation constitutes the newly synthesized parameter. An alternate representation may exhibit mathematical properties that make it more useful for feedback generation—for example, it may convert a vector to its orientation. The representations may include: (i) magnitude with orientation angles, (ii) quaternions (without limitation to unit quaternions), and (iii) radial and rotational (tangential) components of a velocity vector when given the associated position vector. Parameters whose components have the meaning of angles can be equivalently represented as: (i) rotation matrices, (ii) Euler axis and angle, (iii) Euler angles, wherein multiple choices of rotation axes exist (e.g., an alternate set of rotation axes is commonly called Tait-Bryan angles), (iv) quaternions, (v) Cayley-Klein parameters, and (vi) Rodrigues parameters.

Time derivatives and integrals are another technique for deriving the synthetic parameters. A vector's time derivatives and time integrals may be used to convert between position, velocity, acceleration and jerk in terms of both linear and rotational motion. When energy and power is the technique employed for deriving the synthetic parameters, kinetic and kinematic parameters may be combined to derive the energy of a part of the system (the body), or change in energy—the power generated or absorbed by the system. The synthetic parameter derivation technique may also utilize statistical measures. In particular, mean, variance, covariance, and other statistical measures of one or multiple signals may be computed. The measures may be computed over all data since the start of the experiment, or a temporal subset. The temporal subset referenced to the present is also known as a rolling window.

The technique for deriving the synthetic parameters may also comprise curve and surface fitting. The prescribed motion, whether derived from a prior executed motion or arbitrarily specified, can be represented and substituted with a function that best fits such data according to some error minimization criterion. The mathematical representation of a fitting curve or surface can be chosen from the explicit, implicit and parametric representations. Examples of some fitting functions that may be utilized include: (i) scalar-valued and vector-valued polynomials, (ii) Bezier curves and surfaces, (iii) B-Spline curves and surfaces, (iv) non-uniform rational B-spline (NURBS) curves and surfaces, and (v) T-Spline surfaces.

Domain transformations are another technique for deriving the synthetic parameters. The signal can be transformed from the time domain to another domain, such as frequency or quefrency domain. The time-to-frequency transform is called the Fourier transform and yields a spectrum. The time-to-quefrency transform yields a cepstrum. The synthetic parameter derivation technique may also comprise event detection. With this technique, events, found by placing constraints on

parameters, can be marked and their properties constitute a new set of parameters. For example, the temporal or spatial location of maximum (peak) or minimum values can be extracted from the signal. The reversals of motion direction can also be detected. Normalization may also be used as the synthetic parameter derivation technique. A reference motion may be both spatially and temporally normalized. Spatial normalization limits the spatial extent of the motion to arbitrary boundaries, for example within a cube having a unit (1) side length. Temporal normalization limits the duration of the reference motion, for example to one (1) unit of time. The normalization techniques include peak detection, scaling and truncation. The latter two can be either or both spatial and temporal. Finally, the synthetic parameter derivation technique may comprise truncation. That is, parts of the reference motion that are deemed not useful by other criteria can be truncated by either removal of data for given time instants, or constraint of values within chosen bounds. For example, in golf, one may deem unnecessary the data prior to the commencement of ball-directed motion of the putter.

Now, the abstract feedback signal (i.e., the sensory output signal) will be described. While the formed feedback signal is concerned with the manner in which the feedback is delivered to the human user, the abstract feedback signal is concerned with the manner in which the feedback signal is generated or obtained from the motion data. In general terms, the abstract feedback signal $\vec{f}_a(t)$ is a measure of a deviation between the executed motion $\vec{p}(t)$ and the desired, or reference, motion $\vec{w}(t)$. The feedback signal is abstract from the form of the feedback itself to the user. The abstract feedback generation process can be generally described by the flow diagram in FIG. 27. In general, the abstract feedback generation involves following sub-operations: (i) agreement, (ii) comparison, and (iii) adaptation. First, with agreement, the executed motion $\vec{p}(t)$ is brought to the feedback-agreeing form \vec{p}_a . The feedback-agreeing form may be parametrized by an adaptation input \vec{a} . This form agrees with the dimensions, reference frames and units of the reference motion \vec{w} . Secondly, with comparison, the reference motion \vec{w} and the feedback-agreeing form \vec{p}_a is used to compute the abstract feedback \vec{f}_a . The latter can be parametrized by an adaptation input \vec{a} . Thirdly, with adaptation, the executed motion and the reference motion can provide input to an adaptation function $\vec{a}(t)$. The adaptation values are used to adjust the sensitivity, temporal and spatial, alignment and other parameters of the agreement and comparison processes in order to provide useful feedback.

Next, the selection signal $\vec{s}(t)$ will be described. The selection signal $\vec{s}(t)$ is used for selection of the reference motion, the abstract feedback and the formed feedback schemes according to the activity being performed. Because the selection signal generation is performed fundamentally similarly to the abstract feedback generation, it will be described in conjunction with the discussion of the abstract feedback signal. The selection signal $\vec{s}(t)$ allows the system to adjust the one or more parameters of the baseline movement path and/or the velocity profile to accommodate a plurality of different activities performed by the user.

The plurality of different activities performed in succession by the user necessitates the selection of a relevant reference motion, abstract feedback and formed feedback schemes. Such selection from a list of activities, performed

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manually by the trainee, may disrupt the flow of the training. As such, it is beneficial to automate the selection by determining the type of activity being performed without explicit user input to that effect.

The activity matching is accomplished by comparing the executed motion with each reference motion from a set of reference motions, representing the anticipated activities, and selecting the closest match. As such, it is a case of signal classification. In the simplest case, the signal used for such a comparison may be the same as the abstract feedback signal.

In one or more embodiments, each activity in the set of the anticipated activities may optionally be assigned a weight that favors certain selected activities over the others. Such weights may be adjusted to favor the most recently performed activities. This limits the chance of erroneously switching an activity due to an occasionally poor performance that happens to be more similar to some other anticipated activity.

Also, in one or more embodiments, the system incorporates one or more devices that enables the activity selection by an explicit input from the user. For example: providing a "select enable" switch on the club. The selection signal would only be used to switch an activity if the motion was performed with the button being depressed. Another enable mechanism can leverage the choice of the implement used to execute the motion. For example, the use of a golf putter would limit the anticipated activity set to those relevant to putting, whereas the use of a driver club would similarly limit the anticipated activity set to those relevant to drives.

To facilitate the accuracy of the selection process, the selection signal for each anticipated activity can be continuously generated even if the explicit user input bars the selection. Such signal can be used by a machine learning algorithm to further continuously adjust the thresholds used to classify the motion as belonging to a certain anticipated activity.

Now, the agreement sub-operation will be explained in detail. The feedback-agreeing form has the same number of dimensions, and its components have the same units of measurements, as the reference motion. The meaning, or semantics, of the parameters in both forms also typically match, unless a cross-referenced feedback is desired. For example, one can train the motion of one arm to match the motion of another arm. The reference motion's signal applies to the left arm, while the executed motion signal applies to the right arm. The semantic mismatch between them is desirable under the circumstances.

The data provided by the adaptation input can be used to adjust the parameters of the agreement computations. For example, the bandwidth of a filter applied to the motion data may be increased as the trainee's performance improves.

The agreement functions used depend both on the choice of the parameters forming the executed motion, and the parameters forming the reference. The use of synthetic reference parameters may necessitate the computation of the same synthetic parameters from the motion signal during the agreement. Many of the functions useful for the calibration of the executed motion signal can be utilized here as well. For example, scaling may be used to bring the units of measurement into agreement (e.g., the velocity in the reference motion might be represented using the International System of Units (SI units), while the velocity in the captured motion may be expressed in terms of the Mach number obtained from an air probe). As another example, offset removal may be used to bring the zero reference point (intercept) of the executed motion into agreement with the one used for the reference. For example, a reference acceleration signal might not include the 1 g offset due to the acceleration of gravity at the site of the executed motion. As yet another example,

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sensor and component fusion may be used to reduce the dimensionality of vector-valued parameters, or to convert vector-valued parameters to scalar ones. For example, suppose the feedback shall be an indication of how closely a curveball's rotational velocity is to a desired target value. The reference motion consists only of a scalar magnitude of the angular velocity vector. The captured executed motion may consist of the three-dimensional (3D) positions of a set of three reference points on the surface of the ball. The reference point positions, having nine (9) components in all, need to be reduced to a single-component angular velocity. As yet another example, filtering may be used to remove the frequency components of the captured motion that are not deemed useful for the generation of the feedback. For example, a bandpass filter might be used to select the base harmonic of the position of a baton twirler's baton.

Next, the manner in which the movement path and/or the velocity profile of the user is compared to a respective baseline movement path and/or velocity profile will be described. In addition, the manner in which it is determined how closely the movement path and/or the velocity profile of the user conforms to the respective baseline movement path and/or velocity profile will be explained.

While in some embodiments, the feedback's measure of deviation may be a simple mathematical subtraction, in other embodiments, the feedback's measure of deviation may be any function that depends on time itself and the time history of executed motion and reference motion and optional adaptation, such as that represented by the following equation:

$$\vec{f}_a(t) = f(\{\forall_{t_a < \tau < t} : (\vec{p}(\tau), \vec{w}(\tau), \vec{a}(\tau))\}, t) \quad (8)$$

The time history $\{\forall_{t_a < \tau < t} : (\vec{p}(\tau), \vec{w}(\tau), \vec{a}(\tau))\}$ reads a set, for the time $\tau: t_a < \tau < t$ since the start of the experiment (t_a) up to now (t), of the pairs of the executed and reference motions and adaptation, \vec{p} , \vec{w} , and \vec{a} , respectively. The abstract feedback may contain multiple measures of the deviation, derived from one or more reference motions.

Exemplary techniques to compare the executed motion to the reference are explained below. Such computations may be combined, for example, two signals may be subtracted and then a variance of the result computed. Some functions listed below take single parameters. Those functions are used following another operation that has combined the executed and reference parameters.

Subtraction of the executed and reference parameters may be done using one of the following functions:

$$\vec{w} - \vec{p} \text{ or } \vec{w} + \vec{p}, \text{ depending on mutual orientation of vectors,} \quad (9)$$

$$\|\vec{w} - \vec{p}\|, \text{ where } \|\cdot\| \text{ is the Euclidean vector norm,} \quad (10)$$

$$\sqrt{w^2 - p^2}, \text{ where } w \text{ and } p \text{ are scalar,} \quad (11)$$

Cosine Similarity is defined as:

$$\frac{\vec{w} \cdot \vec{p}}{\|\vec{w}\| \|\vec{p}\|}, \quad (12)$$

where " \cdot " is the dot product, and " $\|\cdot\|$ " is the Euclidean norm,

Tanimoto metric is defined as:

$$\frac{\vec{w} \cdot \vec{p}}{\|\vec{w}\|^2 + \|\vec{p}\|^2 - \vec{w} \cdot \vec{p}} \quad (13)$$

where “ \cdot ” is the dot product,

and $\|\cdot\|$ is the Euclidean norm.

Statistical measures of covariance and correlation act on two or more parameters selected from the executed and/or reference motions. The mean and variance act on a single parameter. Convolutional measures are computed by first convolving the executed motion with the reference motion, then applying another self-comparison technique, such as peak detection, to the result. The output of the comparison function constitutes a measure of deviation between the reference and executed motion. Such abstract feedback is then formed and presented to the subject. The scaling of the abstract feedback in relation to the formed feedback may be fixed or adaptive, depending on the task and chosen training strategy.

Hereinafter, the manner in which one or more parameters of the baseline movement path and/or the velocity profile may be adjusted to accommodate at least one of: (i) a skill level of the user with respect to a particular activity, (ii) a particular movement style of the user, and (iii) physical limits of the user, will be described. In addition, the manner in which the sensitivity of the biofeedback is adjusted so as to accommodate users of different skill levels will be explained.

The adaptation signal may be used to adjust the parameters of the agreement and abstract feedback generation operations. It is of use to tune those operations to the skill level of the user with respect to a particular activity, a particular movement style of the user, and his or her physical limits. As illustrated in the signal process flow diagram of FIG. 28, one way of performing parameter adaptation is optimization towards a given goal, given a goal function $\vec{g}(t)$. The goal

function takes the abstract feedback signal $\vec{f}_a(t)$ and optionally the adapted executed motion $\vec{p}_a(t)$, and provides input that steers the adaptation signal towards the goal. This optimization problem, albeit generally nonlinear, may be solved using various known optimization techniques. The goal function must be chosen such that it leads to the feedback that is useful in the training process. It should address the following variability inherent in the execution of the motion: (i) skill level, (ii) movement style, and (iii) physical limits of the user.

Initially, with respect to skill level, the abstract feedback can be used as an estimate of the difficulty of the activity. The goal is to achieve the feedback such that the activity appears, by the feedback provided to the user, to be neither extremely challenging nor extremely easy. This can be achieved by adapting either the gain or the reference feedback level. If the reference level is being adapted, then the gain can be selected to maintain the expected level of variance of the feedback signal, considered within one or more repetitions of the motion.

Secondly, with respect to the movement style, the abstract feedback signal can be dependent on multiple aspects of the motion as well as on multiple aspects of the reference motion, as defined by the different computations that are performed in parallel on the same executed and reference motions to obtain the feedback. Each of those dependencies can be weighted. The weights are subject to adaptation. The weights can be

optimized to minimize the influence of those aspects of the motion that are highly variable and show no ongoing improvement. As other aspects of the motion improve, the weights of such suppressed aspects of the motion can be periodically re-enhanced to probe whether further improvement can be achieved. The schedule of such re-enhancements can be itself optimized to minimize nuisance negative feedback, based on established models of human learning, such as those in the SuperMemo body of work (see e.g., <http://www.supermemo.com/english/algsm11.htm>). If multiple styles of motion performance are a-priori recognized for a given activity, the reference motion can include them in parallel. The goal is to reinforce the one of the multiple styles of reference motion that best approaches the executed motion.

Thirdly, with respect to the physical limits of the user, the abstract feedback for each executed motion has a certain distribution of values across multiple trials. The physical limitations can be extracted as the parameters of those distributions. For example, a performance well under the physical limits may exhibit a symmetric distribution, while a performance at the physical limit may exhibit an asymmetric distribution. The extracted parameters can be used with biomechanically derived models of human performance to quantify one or more aspects of the user's physical limitations. For example, a certain motion may be kinetically limited to a maximum torque due to the cross-section of a key muscle generating the motion. Apart from the muscle's cross section, the biomechanical model may include an estimate of the anaerobically available energy stored in the volume of the muscle. Such energy store is depleted with repeated motions. The estimate can be used to adapt the virtual torque that would have been necessary to produce the reference motion in a similarly built individual.

In the illustrative embodiment, the acquired or captured data may be used to compare the motion to some prescribed form, and to provide real-time feedback to the human user as to possible deviations from the prescribed form. The feedback to the user may be provided by a plurality of different means. These means actuate, or act upon, a formed feedback

signal $\vec{f}_f(t)$. The formed feedback may be specific to given means of presentation. Some of the functions used for calculation of the synthetic reference motion may also form the feedback (e.g., refer to the choice of synthetic parameters explained above). For example, as described above, the feedback may comprise aural or auditory feedback from an auditory sensory output device 60d. In one or more embodiments, the auditory sensory output device(s) 60d may be in the form of headphones, or in the form of sound sources installed on equipment or in the environment the human interacts with (e.g., one or more speakers may be integrated into the sensor unit 22 or the central control unit 24). Also, the sound emitted by the auditory sensory output device 60d may represent one or more feedback signals in one or more of the following exemplary ways: (i) by the timbre/texture of the sound, (ii) by the volume and spatial localization of the sound, (iii) by the pitch and harmonic content, and/or (iv) by the envelope (the attack, sustain, hold and decay aspects of the sound). The formed feedback signal represents the sound pressure over time.

As another example, as also described above, the feedback may comprise visual feedback from a light-based sensory output device 60c or a visual sensory output device 60e. The visual feedback adds or changes the light perceived by the human eye in various ways, such as by modulating the brightness or focus of the perceived scene, using optoelectronic shutters, variable lenses, or augmented reality systems. Such feedback can modify the visual perception by providing

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visual cues not ordinarily present. For example, it can present a stimulus that is temporally or spatially synchronized to the desired event. More specifically, for example, spatially or temporally non-essential aspects of the viewed scene can be defocused, have their contrast reduced, or be blanked out, while the essential aspects of the scene can have their focus, contrast, or color saturation improved. The visual feedback may also add or change the light perceived by the human eye by adding imaged or non-imaged sources of lights that can, for example, prompt for attention, add information related to the external event and/or the performance of the human. The formed feedback signal represents the parameters of the image modulation, the image contents of the augmented reality display, the intensity and color of non-imaged sources of light, etc.

As yet another example, as mentioned above, the feedback may comprise haptic or tactile feedback from a heat-based sensory output device **60a** or a vibratory or vibration-based sensory output device **60b**. This type of feedback exerts tactile and kinetic stimuli (i.e., kinetic stimuli having to do with/of forces). For example, reaction wheel(s) on a golf club or a tennis racket can provide a resisting torque to guide the trajectory of the swing to give a perception of directed resistance not normally experienced. As another example, a force feedback on a piano key can provide timed resistance to guide a player who is learning to play the piano into the proper tempo or rhythm. The haptic sources can actuate based on one or more feedback signals in one or more of the following exemplary ways: (i) by tactile sensations, such as texture, sensation of hot or cold, change in friction (for example by using a controlled vacuum source to control adhesion of skin to the surface), vibration, pressure, etc.; (ii) by force feedback, by imposing additional force and torque loads on the human through the objects the human interacts with. For example, force feedback may be provided by inertial reaction forces and torques, thus it can be exerted on objects that can otherwise freely move through the space, such as bats, clubs, racquets, balls, etc., without having the forces flowing through a structure attached to the ground or the user/performer. The formed feedback signal represents the kinetic and thermodynamic parameters to be actuated.

An exemplary software code that is capable of carrying out some of the fundamental functionality described herein is provided at the end of this written disclosure. The exemplary code generates a simulated executed motion for softball batting, and provides audible feedback for the vertical location of the bat-on-ball. Graphical output generated by the exemplary software code is illustrated in FIGS. 29-35.

In FIGS. 29-31, the bat swing trajectory and the ball trajectory are depicted in graphical form. FIG. 29 illustrates a three-dimensional oblique view of the bat swing and ball trajectory, while FIGS. 30 and 31 illustrate the bat swing and ball trajectory in the Y-Z and X-Y planes, respectively. Initially, referring to the oblique view of FIG. 29, it can be seen that the displacement of the bat throughout the course of the swing is diagrammatically represented by a series of lines **800** (i.e., the motion of the bat is modeled based upon two points disposed on the centerline of the bat). At the beginning of the swing, bat is disposed in an upper, generally vertical position **802**, while at the end of the swing, the bat is disposed in the generally horizontal position **804**. Prior to the end of the swing, in the exemplary motion modeled by the software code, the bat contacts the ball at a point of contact **806**. As shown in FIGS. 29 and 30, prior to contacting the bat, the incoming ball trajectory **808** is generally horizontal. After contacting the bat, the outgoing ball trajectory **810** has a generally diagonal upward path of flight.

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Turning to FIG. 32, a time series plot of the ball y-position and abstract feedback is illustrated. In general, the exemplary software code provided herein determines how closely the ball point of contact coincides with the centerline of the bat. If the ball contacts the bat significantly underneath the bat centerline, then the ball will most likely be directed towards the ground (i.e., a ground ball). Conversely, if the ball contacts the bat significantly above the bat centerline, then the ball will most likely be directed almost straight up in the air (i.e., a pop-up or pop fly). As shown in FIG. 32, the y-position of the ball **812** comprises an approaching portion **814** until the point of contact **806** with the bat, and then a leaving portion **816** following the point of contact with the bat. The time series plot of FIG. 32 further illustrates the abstract feedback approach **818**, an abstract feedback bat centerline to ball center distance curve **820**, and an abstract feedback vertical offset between ball and bat center curve **822**. In order to acquire the bat and ball data required to generate the output illustrated in FIGS. 29-35, a plurality of markers could be provided on the bat and the ball such that the motion of the bat and the ball could be acquired by a marker-based motion tracking system. Alternatively, the bat and the ball could be provided with suitable inertial measurement units and tracking devices disposed thereon, such as those that will be described in conjunction with the scenario of FIG. 19 hereinafter.

In the output of the exemplary software code, the first component of the abstract feedback (f_a) is the bat centerline to ball center distance. The second component of the abstract feedback is the approach flag: true (high value) when the ball is approaching the bat; switches to false (low value) when the ball starts to recede. The third component of the abstract feedback is the vertical offset between center of the ball and the bat centerline. The vertical offset between center of the ball and the bat centerline is used to generate the formed feedback.

In FIG. 33, the bat swing trajectory and the ball trajectory are illustrated together with curves depicting the feedback agreeing form **824**. The feedback agreeing form **824** of the motion is the position of a point on the bat centerline that is closest to the bat. A time series plot of the ball y-position **812'** and the formed feedback signal is illustrated in FIG. 34. The formed feedback is the monaural audio signal that is provided as a feedback to the batter. As shown in FIG. 34, the formed feedback signal comprises a two-tone melody comprising a first reference tone **826** and a second feedback tone **828**. Finally, FIG. 35 illustrates a ball y-position curve **812''**, the feedback signal approach **818'**, the abstract feedback bat centerline to ball center distance curve **820'**, and a curve **822'** illustrating the vertical offset between ball and bat centers, around the time in which the bat contacts the ball (i.e., FIG. 35 is an enlarged view of a portion of FIG. 32 around the time in which the bat contacts the ball).

Now, with reference to FIGS. 19-25, various exemplary scenarios in which the movement assessment system **10** may be utilized to assess athletic performance will be described. For example, as shown in FIG. 19, the movement assessment system **10** described herein may be used to assess the athletic performance of a baseball player **102** that is hitting baseballs **106** being dispensed by an automatic baseball machine **104**. In this scenario **100**, a plurality of motion tracker reference light sources **74a** are provided on the ground surrounding the baseball player **102**. The bat **108**, which is held by the baseball player **102**, is provided with one or more sensor units **22** that at least include an inertial sensor **54a** and a motion tracking sensor **54d**. Also, the baseball player **102** is provided with a central control unit **24** on his torso (e.g., mounted on a

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waistband) that at least includes an inertial sensor **54a**. In addition, the baseball player **102** is provided with a wearable visual display **60e** or a wearable computing device having an optical head-mounted display (OHMD), such as Google® Glass™, for providing visual feedback to the player **102** on his or her performance. Referring again to FIG. 19, it can be seen that the arm of the baseball player **102** that is not holding the bat **108** is provided with a user interface device **76** having at least a display **76b** and a touch input **76c** for controlling the settings of the movement assessment system **10** (e.g., a mobile digital device, such as a smartphone mounted on an armband). The automatic ball machine **104** contains a wireless data interface **110** that enables the ball machine **104** to be controlled by the central control unit **24** worn by the baseball player **102** (e.g., the player **102** is able to adjust the settings of the ball machine **104** by using the user interface device **76**, which is operatively coupled to the central control unit **24**). In this scenario, the movement assessment system **10** is also preferably provided with one or more safety functions that automatically regulate the operation of the baseball machine **104** in the event of an emergency or accident (e.g., when the baseball player **102** has fallen on the ground, the dispensing of baseballs **106** from the baseball machine **104** is automatically stopped).

Another exemplary scenario in which the movement assessment system **10** may be utilized to assess athletic performance is illustrated in FIG. 20. In this scenario **200**, the movement assessment system **10** is used to assess the athletic performance of a downhill skier **202**. The boots **204** of the skier **202** are coupled to the respective skis **206** by virtue of bindings **208** with sensor units **22** incorporated therein. That is, each of the bindings **208** is provided with a sensor unit **22** having at least an inertial sensor **54a** and a load sensor **54c**. Also, as shown in FIG. 20, each of the ski poles **210** is provided with a sensor unit **22** having at least an inertial sensor **54a**. The skier **202** is provided with a central control unit **24** on his torso (e.g., mounted on a waistband) that may include one or more additional sensors, such as an inertial sensor **54a**, etc. As such, the performance of the skier **202** can be analyzed by the movement assessment system **10** during a downhill run or while the skier **202** traverses a cross-country ski course.

In FIGS. 21A and 21B, yet another exemplary scenario in which the movement assessment system **10** may be utilized to assess athletic performance is shown. In this scenario **300**, the movement assessment system **10** is used to assess the athletic performance of a golfer **302** as he or she strikes a golf ball **306** with a golf club **304**. The head **304a** of the golf club **304** is provided with one or more sensor units **22** that at least include an inertial sensor **54a** and a motion tracking sensor **54d**. Also, the golfer **302** is provided with a central control unit **24** on his torso (e.g., mounted on a waistband) that at least includes an inertial sensor **54a**. As shown in FIG. 21A, the golf ball **306** is disposed on a golf tee **308**, which is provided with a motion tracking reference on the shaft thereof, such as a motion tracker reference light source **74a**, a motion tracker reference magnetic signal **74b**, and/or a motion tracker reference ultrasonic signal **74c**. In addition, as best illustrated in FIG. 21B, the golf ball **306** is provided with a plurality of motion tracker reference light sources **74a** dispersed throughout such that some subset of lights are always visible to the motion tracking sensor **54d** on the golf club head **304a**. As such, the golf club **304** is designed to track the golf ball **306** as it comes into proximity with the golf club head **304a**. In FIG. 21A, it can be seen that the golfer **302** is additionally provided with a sensor unit **22** on his or her upper torso (e.g., on the upper chest) having at least an inertial sensor **54a** for detecting the upper

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body movement of the golfer **302** as he or she strikes the ball **306**. Thus, in the scenario **300**, the performance of the golfer **302** may be analyzed by the movement assessment system **10**.

In FIG. 22, still another exemplary scenario in which the movement assessment system **10** may be utilized to assess athletic performance is shown. In this scenario **400**, the movement assessment system **10** is used to assess the athletic performance of a horseback rider **402** as he or she is riding a horse **404**. For the example, the horseback rider **402** may be a jockey and the horse **404** may be a race horse. In such a scenario, the movement assessment system **10** is used to assess the performance of the jockey as he or she rides the horse during a race. As shown in FIG. 22, the saddle **406** disposed on the horse **404** is provided with one or more sensor units **22** that at least include an inertial sensor **54a**. Also, the saddle **406** is provided with a motion tracking reference disposed thereon, such as a motion tracker reference light source **74a**, a motion tracker reference magnetic signal **74b**, and/or a motion tracker reference ultrasonic signal **74c**. In addition, the horseback rider **402** is provided with a central control unit **24** on his torso (e.g., mounted on a band) that at least includes an inertial sensor **54a** and a motion tracking sensor **54d**. Each wrist of the horseback rider **402** is provided with one or more respective sensor units **22** disposed thereon (e.g., mounted on a wristband), which each at least include an inertial sensor **54a** and a motion tracking sensor **54d**. In one or more embodiments, the one or more sensor units **22**, which are disposed on each of the wrists of the horseback rider **402**, detect the motion of the wrists of the horseback rider **402** as he or she manipulates the reins **408**. In FIG. 22, it can be seen that each ankle of the horseback rider **402** is additionally provided with one or more sensor units **22** disposed thereon (e.g., mounted on ankle bands). Each of the one or more sensor units **22** at least includes an inertial sensor **54a** for detecting the motion of the legs of the horseback rider **402** as he or she is riding the horse **404**.

In FIG. 23, yet another exemplary scenario in which the movement assessment system **10** may be utilized to assess athletic performance is shown. In this scenario **500**, the movement assessment system **10** is used to assess the athletic performance of a tennis player **502** as he or she is hitting tennis balls with a tennis racket **504**. The tennis player **502** is provided with a central control unit **24** on his torso (e.g., mounted on a waistband) that at least includes an inertial sensor **54a** and a magnetometer-type sensor **54b**. The central control unit **24** on the torso of the tennis player **502** may also include a wireless data interface **62'** (e.g., in the form of Bluetooth), a wired data interface **64'** for data maintenance and/or charging (e.g., in the form of a USB connection), a power source in the form of a battery **66'**, a wireless power receiver **68'** for charging the battery **66'** of the central control unit **24**, nonvolatile memory **72'**, and user interfaces **76'** in the forms of one or more buttons **76a** and a display **76b**. The handle or throat of the tennis racket **504**, which is held by the tennis player **502**, is provided with one or more sensor units **22** that at least include an inertial sensor **54a** and a magnetometer-type sensor **54b**. Also, the wrist of the tennis player **502** holding the racket is provided with one or more sensor units **22** (e.g., mounted on a wristband) that also at least include an inertial sensor **54a** and a magnetometer-type sensor **54b**. In addition, one or more sensor units **22**, which at least include an inertial sensor **54a** and a magnetometer-type sensor **54b**, are mounted on the headphones **506** of the tennis player **502**. The one or more sensor units **22** on the tennis racket **504**, the wrist of the tennis player **502**, and the headphones **506** of the tennis player **502** may also include a wireless data interface **62** (e.g., in the form of Bluetooth) for

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communicating with the central control unit 24, a power source in the form of a battery 66, and basic user interfaces 76 comprising one or more buttons 76a and a simple display 76b. In addition to the one or more sensor units 22, the headphones 506 worn by the tennis player 502 also include a wireless data interface 62 (e.g., in the form of Bluetooth) for communicating with the central control unit 24, a power source in the form of a battery 66, and an auditory sensory output device 60d (i.e., the headphones 506 may comprise stereo speakers for providing auditory biofeedback to the tennis player 502 as he or she is hitting tennis balls). In one or more embodiments, the headphones 506 are in the form of Bluetooth headphones.

In FIG. 24, still another exemplary scenario in which the movement assessment system 10 may be utilized to assess athletic performance is shown. In this scenario 600, the movement assessment system 10 is used to assess the performance of a person 602 as he or she is flying a handglider 604. As shown in this figure, the handle bar assembly 606 of the handglider 604 is provided with a plurality of motion tracking reference devices thereon, which may be in the form of motion tracker reference light sources 74a, motion tracker reference magnetic signals 74b, and/or motion tracker reference ultrasonic signals 74c. In addition, the handle bar assembly 606 of the handglider 604 is provided with a sensor unit 22 attached thereto, wherein the sensor unit 22 comprises at least an inertial sensor 54a, an air pressure sensor 54f for detecting the atmospheric air pressure, and a global positioning system ("GPS") sensor 54g for detecting the location of the handglider 604. Referring again to FIG. 24, it can be seen that the person 602 flying the handglider 604 is provided with a central control unit 24 on his or her torso (e.g., mounted on a waistband) that at least includes an inertial sensor 54a and a motion tracking sensor 54d. The central control unit 24 on the torso of the person 602 also includes at least non-volatile memory 72' for storing data the measurement data acquired by the plurality of sensing devices (e.g., 54a, 54d). The person 602 on the handglider 604 is additionally provided with a sensor unit 22 on his or her upper torso (e.g., on the upper chest) also having at least an inertial sensor 54a for detecting the upper body movement of the person 602 and a motion tracking sensor 54d for tracking the motion of the upper body of the person 602.

In FIG. 25, yet another exemplary scenario in which the movement assessment system 10 may be utilized to assess athletic performance is shown. In this scenario 700, the movement assessment system 10 is used to assess the athletic performance of a plurality of members 702, 704 of a rowing team that are propelling a row boat 708 using oars 710 disposed on opposite sides of the row boat 708. As shown in this figure, the row boat 708 is provided with a plurality of motion tracker reference light sources 74a disposed on the upper surface thereof dispersed throughout such that some subset of lights is always visible to the motion tracking sensors 54d disposed on the rowing team members 702, 704. In an exemplary embodiment, each of the reference light sources 74a includes a battery 66 and a wireless power receiver 68 for supplying the light emitting devices (e.g., light emitting diodes or LEDs) of the reference light sources 74a with power. While a total of six (6) motion tracker reference light sources 74a are shown on the upper surface of the row boat 708 in FIG. 25, it is to be understood that any suitable quantity of reference light sources 74a may be used as long as at least some of the reference light sources 74a are visible to the motion tracking sensors 54d.

With reference again to FIG. 25, it can be seen that each of the oars 710 is provided with a sensor unit 22 disposed thereon. Each of the sensor units 22 includes at least an

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inertial sensor 54a and a load sensor 54c for measuring the oar loading. Also, each oar sensor unit 22 may comprise a power source in the form of a battery 66, a wireless power receiver 68 for charging the battery 66 of the sensor unit 22, non-volatile memory 72 for storing data the measurement data acquired by the plurality of sensing devices (e.g., 54a, 54c), a wireless data interface 62 (e.g., in the form of Bluetooth) for communicating with the central control unit 24 on each respective rower 702, 704, and a user interface 76 in the form of a display 76b. As shown in FIG. 25, each rower 702, 704 is provided with a central control unit 24 that includes a wireless data interface 62' in the form of Bluetooth and Wi-Fi (i.e., wireless local area networks). Each rower 702, 704 is additionally provided with a sensor unit 22 on his upper torso (i.e., on the upper chest) also having at least an inertial sensor 54a for detecting the upper body movement of the rower 702, 704 and a motion tracking sensor 54d for tracking the motion of the upper body of the rower 702, 704. Each upper torso sensor unit 22 may also comprise at least a power source in the form of a battery 66, a wireless power receiver 68 for charging the battery 66 of the sensor unit 22, and a wireless data interface 62 (e.g., in the form of Bluetooth) for communicating with the central control unit 24 on each respective rower 702, 704, and a user interface 76 in the form of a display 76b. In one or more embodiments, the sensor units 22 on the oars 710 held by the first rowing team member 702 wirelessly communicate with the central control unit 24 disposed on the first rowing team member 702 by means of Bluetooth. The upper torso sensor unit 22 on the first rowing team member 702 also communicates with the central control unit 24 disposed on the first rowing team member 702 by means of Bluetooth. Similarly, the sensor units 22 on the oars 710 held by the second rowing team member 704, and the upper torso sensor unit 22 on the second rowing team member 704, wirelessly communicate with the central control unit 24 disposed on the second rowing team member 704 by means of Bluetooth. Each of the central control units 24 that are disposed on the first and second rowing team members 702, 704 wirelessly communicate with the tablet 712 held by the rowing team instructor or captain 706 by Wi-Fi. As such, the rowing team instructor or captain 706 is able to continually monitor the performance of the rowing team members 702, 704 as they are propelling the row boat 708 on a body of water, such as a river, lake, or reservoir.

In addition for being used to analyze athletic performance, it is to be understood that the movement assessment apparatus or system 10 described herein may also be utilized to analyze the balance and gait of an individual undergoing rehabilitation. For example, suppose an individual sustained an injury that has adversely affected his or her balance, the movement assessment apparatus or system 10 described herein may be used to assess the progress of his or her rehabilitation.

As one example of a rehabilitative application, in some embodiments, the movement assessment apparatus or system 10, which is shown in FIGS. 1 and 2, is used to determine positional data (i.e., three-dimensional coordinates) and/or a velocity profile for one or more body gestures of the subject or patient during the performance of a task of daily living. The one or more body gestures of the subject or patient may comprise at least one of: (i) one or more limb movements of the patient, (ii) one or more torso movements of the patient, and (iii) a combination of one or more limb movements and one or more torso movements of the patient. For example, one such task of daily living may comprise a scenario wherein a patient is walking along a prescribed path (e.g., a straight-line extending a predetermined distance). While the patient is performing this task of daily living, the movement assessment apparatus 10 may analyze the performance of the patient

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during the execution of this task, and then provide appropriate real-time feedback to the patient regarding his or her performance. In particular, one or more sensor units 22 of the movement assessment apparatus 10 may be coupled to each of the patient's legs such that the motion of the patient's legs may be detected. Then, the data processing device (e.g., 52, 52') of the movement assessment apparatus 10 may be used to determine the movement paths or velocity profiles for each of the patient's legs by using the output signals of the one or more sensor units 22. After which, the data processing device (e.g., 52, 52') of the movement assessment apparatus 10 may compare the movement paths and/or the velocity profiles determined for each of the patient's legs to respective baseline movement paths and/or velocity profiles (e.g., to baseline movement paths or baseline velocity profiles for an individual having a normal gait pattern) and determine how closely the movement paths and/or the velocity profiles determined for the legs of the patient conform to the respective baseline movement paths and/or baseline velocity profiles. After performing the comparison of the movement paths and/or the velocity profiles determined for each of the patient's legs to respective baseline movement paths and/or velocity profiles, the data processing device (e.g., 52, 52') of the movement assessment apparatus 10 generates a sensory output signal based upon the conformity of the movement paths and/or velocity profiles for each of the patient's legs to the respective baseline movement paths and/or velocity profiles so that the appropriate biofeedback may be delivered to the patient. As such, based upon a comparison of the patient's actual leg movement paths and/or velocity profiles to the baseline movement paths and/or velocity profiles, a physical therapist treating the subject or patient may conclude that the subject's condition is improving over time. Thus, advantageously, the movement assessment apparatus or system 10 enables a subject's movement to be analyzed during a task of daily living so that a determination can be made as to whether or not the subject's gait is improving.

Although the invention has been shown and described with respect to a certain embodiment or embodiments, it is apparent that this invention can be embodied in many different forms and that many other modifications and variations are possible without departing from the spirit and scope of this invention. Moreover, while reference is made throughout this disclosure to, for example, "an illustrative embodiment", "an exemplary embodiment", "one embodiment" or a "further embodiment", it is to be understood that some or all aspects of these various embodiments may be combined with another as part of an overall embodiment of the invention.

In addition, while exemplary embodiments have been described herein, one of ordinary skill in the art will readily appreciate that the exemplary embodiments set forth above are merely illustrative in nature and should not be construed as to limit the claims in any manner. Rather, the scope of the invention is defined only by the appended claims and their equivalents, and not, by the preceding description.

Exemplary Source Code

The exemplary source code provided below generates a simulated executed motion for softball batting, and provides audible feedback for the vertical location of the bat-on-ball. The feedback is provided after the bat has contacted the ball. While the exemplary source code is written particularly for Octave 3.6 (see <http://octave.sf.net>), it is to be understood that this source code can be readily adapted for other computer programming languages.

In the exemplary code, the executed motion is the position of the center of the ball, and the position of two points on the centerline of the bat. The reference motion is the ball center

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position taken directly from the executed motion. The feedback-agreeing form is the position of a point on the bat centerline closest to the ball.

In the exemplary code provided below, the abstract feedback comprises the following elements: (1) instantaneous closest distance between bat centerline and ball center, (2) an approach flag, which is set true when the ball distance is decreasing, and which is set false when the distance is increasing after a strike or miss, and (3) a vertical component of the distance between the bat centerline and the ball center.

The formed feedback generated by the exemplary code comprises a two tone melody, starting after the approach flag turns false. The first tone is a reference tone, the second tone is higher or lower compared to the reference depending on how high or low the hit was with relation to the center of the ball. The first tone lasts 250 ms, the second tone lasts 400 ms.

In the exemplary code provided below, a right-handed coordinate system is utilized, wherein the z axis points straight up, and the x and y axes are in the horizontal plane. At the point of contact, z=0, solely for convenience in simulating the motion capture. All measurements in the exemplary code are in SI units (meters, seconds, etc.).

The exemplary source code is as follows:

```
%
% Example of Feedback Generation
% Batting Contact Location, release 06/19/2014%
% written for Octave 3.6, see http://octave.sf.net
%
% Activity: softball batting
% All positions are 3D in ground reference frame unless
% stated otherwise.
% Executed Motion: position of the center of the ball,
% position of two points
% on the centerline of the bat.
% Reference Motion: ball center position taken directly
% from the executed motion.
% Feedback-agreeing form:
% Position of a point on the bat centerline closest to the
% ball.
% Abstract Feedback:
% 1. Instantaneous closest distance between bat centerline
% and ball center.
% 2. Approach flag: true when the ball distance is decreasing, false when the
% distance is increasing after a strike or miss.
% 3. Vertical component of the distance between the bat
% centerline and the ball
% center.
% Formed Feedback:
% A two tone melody, starting after the approach flag turns
% false. The first
% tone is a reference tone, the second tone is higher or
% lower compared to
% the reference depending on how high/low the hit was
% with relation to the
% center of the ball. First tone lasts 250 ms, second tone
% lasts 400 ms.
%
% Coordinate system: Right-handed system, z points
% straight up, x and y are
% in the horizontal plane. z=0 is at the point of contact,
% solely for
% convenience in simulating the motion capture.
%
% All measurements are in SI units (meters, seconds).
setenv GNUTERM qt
pkg load linear-algebra geometry audio signal
```

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```

global deg=pi/180; % One degree of angle in radians
global sound_play_utility='/opt/local/bin/play -q -t AU -';
global f_factor=16;
% The formed feedback is sampled at 16 times the sam-
    pling rate
% of the motion, since its frequency content is much higher
% than that of the motion.
%% Simulate an Executed Motion
global p_i p_o p_o_unit
function p=bat(t)
    global deg
    bat_in=[-0.5 0 0]'; % inner point on the bat
    bat_out=[-1.1 0 0]'; % outer point on the bat
    bat_in_sweep=100*deg; % sweep angle of inner bat
    point
    bat_out_sweep=160*deg; % sweep angle of outer bat
    point
    swing_incl=-90*deg; % initial inclination of the swing
    plane
    N=length(t);
    t(t<0)=0;
    t(t>1.2)=1.2;
    t1=t;
    t1(t1>1)=1;
    bat_in_angle=(1-t).*bat_in_sweep;
    bat_out_angle=(1-t).*bat_out_sweep;
    swing_incl=(1-t1)*swing_incl;
    axis=reshape(rotv([1 0 0], swing_incl)*[0 0 1]', 3, N);
    global p_i p_o p_o_unit
    p_i=reshape(rotv(axis', bat_in_angle)*bat_in, 3, N);
    p_o=reshape(rotv(axis', bat_out_angle)*bat_out, 3, N);
    p_o_unit=(p_o-p_i).*(1/11)*(1./norm(p_o-p_i, 'col-
        umns'));
    p_o=p_i+p_o_unit*norm(bat_out-bat_in);
    p=[p_i; p_o];
end
function p=ball(t)
    global deg
    ball_offset=[0 0 .015]'; % contact point offset
    x_incl_in=0.5*deg; % incoming inclination
    x_incl_out=15*deg; % outgoing inclination
    v_in=10; % incoming velocity
    v_out=20; % outgoing velocity
    N=length(t);
    t_in=t<=1;
    t_out=t>=1;
    p_in=(rotv([1 0 0], x_incl_in)*[0 -1 0])*(t_in.*(1-t)
        *v_in);
    p_out=(rotv([1 0 0], x_incl_out)*[0 -1 0])*(t_out.*(1-
        1)*v_out);
    p=p_in+p_out+[-1 0 0]'+ball_offset;
end
T=0.2; % Assume a swing lasts 0.2 s from the highest point
    to contact
global tau=1/1000; % Sample at 1000 Hz
t=-0.3:(tau/T):1.5; % A parameter that goes from 0 to 1
    over the duration of
    % the swing. This is *not* time. It is sampled at the
    % sampling frequency.
p=[bat(t); ball(t)];
%% Calculate Reference Motion
w=p(:, 7:9);
%% Calculate Feedback Agreeing Form
function pa=gen_pa(p)
    bat1=p(:, 1:3);
    bat2=p(:, 4:6);
    ball=p(:, 7:9);

```

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```

% A plane normal to the bat, passing through the ball.
normal=bat2-bat1;
plane=createPlane(ball, normal);
% The intersection of the plane and the bat is the point
    closest to the ball
pa=intersectLinePlane([bat1 normal], plane);
end
pa=gen_pa(p);
%% Calculate Abstract Feedback
function fa=gen_fa(pa, w)
    % Instantaneous closest distance between bat centerline
    and ball center.
    bat_ball=distancePoints(pa, w, 'diag');
    % True when the ball distance is decreasing, false when
    the
    % distance is increasing after a strike or miss. The value
    is locked out
    % at true when the distance from bat midpoint to the ball
    exceeds 0.5 m.
    approach=[1; (bat_ball(2:end)<=bat_ball(1:end-1))|
        (bat_ball(2:end)>0.5)];
    % Vertical component of the distance between the bat
    centerline and the ball
    % center.
    vert=w(:,3)-pa(:,3);
    fa=[bat_ball approach vert];
end
fa=gen_fa(pa, w);
%% Calculate Formed Feedback
function ff=gen_ff(fa)
    global tau f_factor
    ftau=tau/f_factor;
    T1=0.25; % duration of the reference tone
    f1=440; % frequency of the reference tone
    T2=0.4; % duration of the feedback tone
    sens=40/0.01; % feedback sensitivity in Hz/m of dis-
        placement
    % Index at which the formed feedback should start
    start_idx=(find(!fa(:,2)))(1)-1)*f_factor;
    ff=zeros(start_idx+(T1+T2)/ftau, 1);
    f2=f1+sens*fa(start_idx/f_factor, 3); % frequency of the
        feedback tone
    if f2<50
        f2=50;
    end
    N1=T1*f1; % number of periods of the reference tone
    n1=floor(T1/ftau); % number of samples of the refer-
        ence tone
    N2=T2*f2; % number of periods of the feedback tone
    n2=floor(T2/ftau); % number of samples of the feedback
        tone
    ff(start_idx:start_idx+n1)=0.9*sawtooth(0:(2*pi*N1)/
        n1:(2*pi*N1), 0.5);
    ff(start_idx+n1:start_idx+n1+n2)=0.9*sawtooth(0:
        (2*pi*N2)/n2:(2*pi*N2), 0.5);
end
ff=gen_ff(fa);
%% Utilities
%%
function plot3d(varargin)
    args={ };
    for i=1:length(varargin)
        arg=varargin{i};
        if (ismatrix(arg) && !ischar(arg) && !isscalar(arg))
            args={args{:,}, arg(1:3:end,:), arg(2:3:end,:), arg
                (3:3:end,:)};
        end
    end

```

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```

else
    args={args{:}, arg};
end
end
plot3(args{:});
end
%% Generate Plots
%
for i=0:1
    f=figure;
    c=get(f, 'colormap');
    set(f, 'colormap', c*0);
    plot3d(p(1:4:end,1:6)', p(:,7:9)', '-');
    axis([-1.5 1.5 -1.5 1.5 -0.2 1])
    view(-50,30);
    set(get(f, 'children'), 'fontname', 'Helvetica');
    if (i)
        xlabel 'X'
        ylabel 'Y'
        zlabel 'Z'
        title 'Oblique View of the Bat Swing and Ball Trajectory'
        text(-.5,.55,-.35, 'incoming ball trajectory')
        text(0.7,.9,-.18, 'outgoing ball trajectory')
        print plot1ann.pdf
    else
        print -mono plot1.pdf
    end
end
for i=0:1
    f=figure;
    plot(p(1:4:end, [2 5])', p(1:4:end, [3 6])', 'k',
        p(1:4:end, 8), p(1:4:end, 9), 'k-');
    set(gca, 'xdir', 'reverse');
    axis([-0.5 1.2 -0.2 1])
    axis square equal
    grid on
    set(get(f, 'children'), 'fontname', 'Helvetica');
    if (i)
        xlabel 'Y'
        ylabel 'Z'
        text(-.1,.15, 'outgoing ball trajectory')
        text(-.1,-.05, 'incoming ball trajectory')
        title 'YZ plane view of the bat swing and ball trajectory'
        print plot2ann.pdf
    else
        print plot2.pdf
    end
end
for i=0:1
    f=figure;
    plot(p(1:4:end, [1 4])', p(1:4:end, [2 5])', 'k', p(1:4:end,
        7), p(1:4:end, 8), 'k-');
    axis([-1.3 1.7 -1.2 1.3])
    axis square equal
    grid on
    set(get(f, 'children'), 'fontname', 'Helvetica');
    if (i)
        xlabel 'X'
        ylabel 'Y'
        text(-.95,-1, 'ball trajectory')
        title 'XY plane view of the bat swing and ball trajectory'
        print -solid -mono plot3ann.pdf
    else
        print plot3.pdf

```

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```

end
end
for i=0:1
    f=figure;
    5 plot(t*T, p(:,8), t*T, fa(:,1), t*T, fa(:,2), t*T, fa(:,3));
    axis([0 0.3 -10 10])
    grid on
    set(get(f, 'children'), 'fontname', 'Helvetica');
    if (i)
        10 legend('ball Y position', 'f_a bat centerline to ball
            center distance',
            'f_a approach', 'f_a vertical offset between ball and
            bat centers');
        xlabel 'time [s]';
        15 title 'Time series plot of ball Y position and abstract
            feedback';
        print plot4ann.pdf
    else
        print plot4.pdf
    end
end
for i=0:1
    f=figure;
    20 plot3d(p(1:4:end,1:6)', p(:,7:9)', 'k-', pa(:,1:3)', 'ko',
        'markersize', 0.75);
    axis([-1.5 1.5 -1.5 1.5 -0.2 1])
    view(-50,30);
    set(get(f, 'children'), 'fontname', 'Helvetica');
    if (i)
        30 xlabel 'X'
        ylabel 'Y'
        zlabel 'Z'
        text(-.5,.55,-.35, 'incoming ball trajectory')
        text(0.7,.9,-.18, 'outgoing ball trajectory')
        35 title(['Oblique View of the Bat Swing, Ball Trajectory
            and the Feedback'
            'Agreeing Form']);
        print plot5ann.pdf
    else
        40 print -mono -dashed plot5.pdf
    end
end
for i=0:1
    f=figure;
    45 t0=t(1)*T;
    plot(t*T, p(:,8), t0:tau/f_factor:t0+(rows(ff)-1)*tau/
        f_factor, ff);
    axis([0.1 0.9 -2 2])
    grid on
    50 set(get(f, 'children'), 'fontname', 'Helvetica');
    if (i)
        legend('ball Y position', 'f_f formed feedback');
        xlabel 'time [s]';
        title 'Time series plot of ball Y position and formed
            feedback';
        55 print plot6ann.pdf
    else
        print -mono plot6.pdf
    end
end
for i=0:1
    f=figure;
    plot(t*T, p(:,8), 'k-', t*T, fa(:,1), 'k-', t*T, 0.1*fa(:,2), '<',
        t*T, fa(:,3), 'k-');
    65 axis([0.19 0.21 -0.5 0.5])
    grid on
    set(get(f, 'children'), 'fontname', 'Helvetica');

```

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```

if (i)
    legend('ball Y position', 'f_a bat centerline to ball
        center distance',
        'f_a approach', 'f_a vertical offset between ball and
        bat centers');
    xlabel 'time [s]';
    title 'Time series plot of ball Y position and abstract
        feedback';
    print plot7ann.pdf
else
    print plot7.pdf
end
end
end

```

The invention claimed is:

1. A movement assessment apparatus configured to provide biofeedback to a user regarding one or more bodily movements executed by the user, the movement assessment apparatus comprising:

at least one sensing device, the at least one sensing device comprising one or more sensors for detecting the motion of a body portion of a user and outputting one or more signals that are generated based upon the motion of the body portion of the user, the at least one sensing device further comprising attachment means for attaching the at least one sensing device to the body portion of the user; a data processing device operatively coupled to the at least one sensing device, the data processing device configured to receive the one or more signals that are output by the one or more sensors of the at least one sensing device, and to determine executed motion data for an executed motion of the body portion of the user using the one or more signals, the data processing device configured to automatically select a reference motion by comparing the executed motion of the body portion of the user to each of a plurality of reference motions representing a plurality of different activities, the data processing device further configured to: (i) execute an agreement operation by converting the executed motion data to a feedback-agreeing form that agrees with at least one of the dimensions, reference frames, and units of baseline motion data of the reference motion, (ii) execute a comparison operation by comparing the feedback-agreeing form of the executed motion data to the baseline motion data of the reference motion, and (iii) determine how closely the feedback-agreeing form of the executed motion data conforms to the baseline motion data of the reference motion, the data processing device additionally configured to generate an abstract feedback signal based upon the execution of the comparison operation; and

a sensory output device operatively coupled to the data processing device, the sensory output device configured to generate a formed feedback signal for delivery to the user that is based upon the abstract feedback signal, the formed feedback signal comprising at least one of a visual indicator, an audible indicator, and a tactile indicator, and the sensory output device further configured to output the at least one of the visual indicator, the audible indicator, and the tactile indicator to the user in order to provide biofeedback as to conformity of the executed motion data to the baseline motion data of the reference motion.

2. The movement assessment apparatus according to claim 1, wherein the one or more sensors of the at least one sensing device comprise at least one of: (i) an accelerometer, (ii) a gyroscope, and (iii) a geomagnetic sensor.

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3. The movement assessment apparatus according to claim 1, wherein the at least one sensing device comprises a plurality of sensing devices, a first of the plurality of sensing devices configured to be attached to a limb of the user, a second of the plurality of sensing devices configured to be attached to a first torso location of the user, a third of the plurality of sensing devices configured to be attached to a head of the user, and a fourth of the plurality of sensing devices configured to be attached to a second torso location of the user.

4. The movement assessment apparatus according to claim 1, wherein the attachment means of the at least one sensing device comprises a resilient band for attaching the at least one sensing device to one of a limb of the user, a torso of the user, and a head of the user.

5. The movement assessment apparatus according to claim 1, wherein the data processing device comprises a microprocessor.

6. The movement assessment apparatus according to claim 1, further comprising a band for attaching the data processing device to a torso of the user.

7. The movement assessment apparatus according to claim 1, wherein the sensory output device comprises an audio headset configured to be worn on a head of the user, and wherein the audio headset is configured to generate the audible indicator that provides biofeedback as to the conformity of the executed motion data to the baseline motion data of the reference motion.

8. The movement assessment apparatus according to claim 1, wherein the at least one sensing device further comprises one or more additional sensors for detecting at least one of: (i) a position of the user, (ii) a body parameter of the user, and (iii) an environmental parameter.

9. The movement assessment apparatus according to claim 8, wherein the one or more additional sensors of the at least one sensing device comprise at least one of: (i) a global positioning system sensor for detecting a position of the user, (ii) a body oxygenation sensor for detecting an oxygen level or oxygen saturation level of the user, (iii) a body temperature sensor for detecting a body temperature of the user, (iv) an ambient temperature sensor for detecting a temperature of an environment in which the user is disposed, and (v) a humidity sensor for detecting a humidity level of the environment in which the user is disposed.

10. The movement assessment apparatus according to claim 1, wherein the sensory output device comprises a light emitting device configured to be worn by the user, and wherein the light emitting device is configured to generate the visual indicator that provides biofeedback as to the conformity of the executed motion data to the baseline motion data of the reference motion.

11. The movement assessment apparatus according to claim 1, wherein the sensory output device comprises a vibratory device configured to be worn by the user, and wherein the vibratory device is configured to generate the tactile indicator that provides biofeedback as to the conformity of the executed motion data to the baseline motion data of the reference motion.

12. The movement assessment apparatus according to claim 1, wherein the baseline motion data of the reference motion includes a baseline movement path and/or a baseline velocity profile, and one or more parameters of the baseline movement path and/or the baseline velocity profile are adjustable so as to accommodate at least one of: (i) a plurality of different activities performed by the user, (ii) a skill level of

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the user with respect to a particular activity, (iii) a particular movement style of the user, and (iv) physical limits of the user.

13. The movement assessment apparatus according to claim 1, further comprising means for adjusting a sensitivity of the biofeedback provided by the apparatus so as to accommodate users of different skill levels.

14. The movement assessment apparatus according to claim 1, wherein the movement assessment apparatus is configured to provide real-time biofeedback to the user.

15. The movement assessment apparatus according to claim 1, wherein the data processing device is further configured to assign weights to the plurality of different activities so as to increase a likelihood that certain ones of the plurality of different activities are selected over other ones of the plurality of different activities.

16. The movement assessment apparatus according to claim 1, further comprising a club with a selection switch disposed thereon for enabling a user to select a particular one of the plurality of different activities that is used by the data processing device to determine the reference motion that is compared to the executed motion of the body portion of the user.

17. The movement assessment apparatus according to claim 1, wherein the data processing device is further configured to execute an adaptation operation whereby one or more parameters of the agreement and comparison operations are adjusted so as to provide biofeedback tailored to at least one of a skill level, movement style, and physical limits of the user; and wherein the data processing device is additionally configured to generate the abstract feedback signal based upon the execution of the adaptation operation.

18. The movement assessment apparatus according to claim 1, wherein the data processing device is further configured to utilize a selection signal for automatically selecting the reference motion, the abstract feedback signal, and the formed feedback signal based upon an activity being performed by the user; and wherein the executed motion data includes a movement path and/or a velocity profile, the selection signal enabling the data processing device to adjust the one or more parameters of the baseline movement path and/or the velocity profile to accommodate a plurality of different activities performed by the user.

19. A method for providing biofeedback to a user regarding one or more bodily movements executed by the user, the method comprising the steps of:

providing a movement assessment apparatus configured to be worn by a user, the movement assessment apparatus including:

at least one first sensing device, the at least one first sensing device comprising one or more sensors for detecting the motion of a body portion of a user and outputting one or more first signals that are generated based upon the motion of the body portion of the user, the at least one first sensing device further comprising first attachment means for attaching the at least one first sensing device to the body portion of the user;

at least one second sensing device, the at least one second sensing device comprising one or more sensors for detecting the motion of an object manipulated by the user and outputting one or more second signals that are generated based upon the motion of the object manipulated by the user, the at least one second sensing device further comprising second attachment means for attaching the at least one second sensing device to the object;

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a data processing device operatively coupled to the at least one first sensing device and the at least one second sensing device, the data processing device configured to receive the one or more first signals that are output by the one or more sensors of the at least one first sensing device, and to determine executed motion data for an executed motion of the body portion of the user using the one or more first signals, the data processing device configured to receive the one or more second signals that are output by the one or more sensors of the at least one second sensing device, and to determine a motion of the object using the one or more second signals, the data processing device further configured to: (i) execute an agreement operation by converting the executed motion data to a feedback-agreeing form that agrees with at least one of the dimensions, reference frames, and units of baseline motion data of a reference motion, (ii) execute a comparison operation by comparing the feedback-agreeing form of the executed motion data to the baseline motion data of the reference motion, and (iii) determine how closely the feedback-agreeing form of the executed motion data conforms to the baseline motion data of the reference motion, the data processing device additionally configured to generate an abstract feedback signal based upon the execution of the comparison operation; and

a sensory output device operatively coupled to the data processing device, the sensory output device configured to generate a formed feedback signal for delivery to the user that is based upon the abstract feedback signal, the formed feedback signal comprising at least one of a visual indicator, an audible indicator, and a tactile indicator, and the sensory output device further configured to output the at least one of the visual indicator, the audible indicator, and the tactile indicator to the user in order to provide biofeedback as to conformity of the executed motion data to the baseline motion data of the reference motion;

outfitting a user with the movement assessment apparatus, which includes attaching the first attachment means of the at least one first sensing device to a body portion of the user;

attaching the second attachment means of the at least one second sensing device to an object;

instructing the user to perform an activity where the user displaces both the body portion with the at least one first sensing device attached thereto and the object with the at least one second sensing device attached thereto;

detecting, by utilizing the at least one first sensing device, the motion of the body portion of the user and outputting one or more first signals that are generated based upon the motion of the body portion of the user;

detecting, by utilizing the at least one second sensing device, the motion of the object manipulated by the user and outputting one or more second signals that are generated based upon the motion of the object manipulated by the user;

receiving, at the data processing device, the one or more first signals that are output by the one or more sensors of the at least one first sensing device and the one or more second signals that are output by the one or more sensors of the at least one second sensing device;

determining, by using the data processing device, executed motion data for an executed motion of the body portion of the user using the one or more first signals;

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determining, by using the data processing device, a motion of the object using the one or more second signals;
 executing an agreement operation, by using the data processing device, whereby the executed motion data is converted to a feedback-agreeing form that agrees with at least one of the dimensions, reference frames, and units of baseline motion data of a reference motion,
 executing a comparison operation, by using the data processing device, whereby the feedback-agreeing form of the executed motion data is compared to the baseline motion data of the reference motion;
 determining, by using the data processing device, how closely the feedback-agreeing form of the executed motion data conforms to the baseline motion data of the reference motion;
 generating, by using the data processing device, an abstract feedback signal based upon the execution of the comparison operation;
 generating, by using the sensory output device, a formed feedback signal for delivery to the user that is based upon the abstract feedback signal, the formed feedback signal comprising at least one of a visual indicator, an audible indicator, and a tactile indicator; and
 outputting the at least one of the visual indicator, the audible indicator, and the tactile indicator from the sensory output device to the user in order to provide quasi-instantaneous, real-time biofeedback as to conformity of the executed motion data to the baseline motion data of the reference motion.

20. The method according to claim **19**, wherein the data processing device is further configured to execute an adaptation operation whereby one or more parameters of the agreement and comparison operations are adjusted so as to provide biofeedback tailored to at least one of a skill level, movement style, and physical limits of the user; and wherein the data processing device is additionally configured to generate the abstract feedback signal based upon the execution of the adaptation operation.

21. The method according to claim **19**, wherein the data processing device is further configured to utilize a selection signal for automatically selecting the reference motion, the abstract feedback signal, and the formed feedback signal based upon an activity being performed by the user; and wherein the executed motion data includes a movement path and/or a velocity profile, the selection signal enabling the data processing device to adjust the one or more parameters of the baseline movement path and/or the velocity profile to accommodate a plurality of different activities performed by the user.

22. A movement and performance assessment apparatus configured to provide biofeedback to a user regarding one or more bodily movements executed by the user, the movement and performance assessment apparatus comprising:

at least one sensing device, the at least one sensing device comprising one or more first sensors for detecting the motion of a body portion of a user and outputting one or more first signals that are generated based upon the motion of the body portion of the user, the at least one sensing device further comprising a plurality of second sensors for detecting an environmental parameter of an environment in which the user is disposed and at least one of: (i) a position of the user, and (ii) a body parameter of the user, the plurality of second sensors outputting one or more second signals, and the at least one sensing device additionally comprising attachment means for attaching the at least one sensing device to the body portion of the user;

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a data processing device operatively coupled to the at least one sensing device, the data processing device configured to receive the one or more first signals that are output by the one or more first sensors of the at least one sensing device, to receive the one or more second signals that are output by the plurality of second sensors of the at least one sensing device, and to determine executed motion data for an executed motion of the body portion of the user using the one or more first signals and to determine an environmental parameter of an environment in which the user is disposed using the one or more second signals, the data processing device configured to automatically select a reference motion by comparing the executed motion of the body portion of the user to each of a plurality of reference motions representing a plurality of different activities, the data processing device further configured to: (i) execute an agreement operation by converting the executed motion data to a feedback-agreeing form that agrees with at least one of the dimensions, reference frames, and units of baseline motion data of the reference motion, (ii) execute a comparison operation by comparing the feedback-agreeing form of the executed motion data to the baseline motion data of the reference motion, and (iii) determine how closely the feedback-agreeing form of the executed motion data conforms to the baseline motion data of the reference motion in order to assess a performance of the user, the data processing device further configured to automatically track the performance of the user based on the environmental parameter of the environment in which the user is disposed, the data processing device additionally configured to generate an abstract feedback signal based upon the execution of the comparison operation; and

a sensory output device operatively coupled to the data processing device, the sensory output device configured to generate a formed feedback signal for delivery to the user that is based upon the abstract feedback signal, the formed feedback signal comprising at least one of a visual indicator, an audible indicator, and a tactile indicator, and the sensory output device further configured to output the at least one of the visual indicator, the audible indicator, and the tactile indicator to the user in order to provide biofeedback as to conformity of the executed motion data to the baseline motion data of the reference motion.

23. The movement and performance assessment apparatus according to claim **22**, wherein the plurality of second sensors of the at least one sensing device comprise at least one of: (i) a global positioning system sensor for detecting a position of the user, (ii) a body oxygenation sensor for detecting an oxygen level or oxygen saturation level of the user, and (iii) a body temperature sensor for detecting a body temperature of the user, and at least one of: (i) an ambient temperature sensor for detecting a temperature of an environment in which the user is disposed, and (ii) a humidity sensor for detecting a humidity level of the environment in which the user is disposed.

24. The movement and performance assessment apparatus according to claim **22**, further comprising a remote computing device operatively coupled to the movement and performance assessment apparatus, the remote computing device comprising a data storage device for storing data acquired by the movement and performance assessment apparatus, the remote computing device further comprising a data processing device for analyzing the data acquired by the movement and performance assessment apparatus.

25. The movement and performance assessment apparatus according to claim 22, further comprising a counting device configured to measure a number of repetitions of an activity performed by the user, the counting device operatively coupled to the data processing device so that the measured number of repetitions are capable of being used in a performance analysis of the user. 5

26. The movement and performance assessment apparatus according to claim 22, wherein the data processing device is further configured to execute an adaptation operation 10 whereby one or more parameters of the agreement and comparison operations are adjusted so as to provide biofeedback tailored to at least one of a skill level, movement style, and physical limits of the user; and wherein the data processing device is additionally configured to generate the abstract 15 feedback signal based upon the execution of the adaptation operation.

27. The movement and performance assessment apparatus according to claim 22, wherein the data processing device is further configured to utilize a selection signal for automatically selecting the reference motion, the abstract feedback signal, and the formed feedback signal based upon an activity being performed by the user; and wherein the executed motion data includes a movement path and/or a velocity profile, the selection signal enabling the data processing device 25 to adjust the one or more parameters of the baseline movement path and/or the velocity profile to accommodate a plurality of different activities performed by the user.

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